Published in partnership with Nanjing Tech University



https://doi.org/10.1038/s41528-024-00311-5

Active electronic skin: an interface towards ambient haptic feedback on physical surfaces

Check for updates

Yuan Guo^{1,2,4}, Yun Wang^{1,2,4}, Qianqian Tong^{3,4}, Boxue Shan^{1,2}, Liwen He^{1,2}, Yuru Zhang^{1,2} & Dangxiao Wang $0^{1,2,3}$

In the era of ubiquitous computing with flourished visual displays in our surroundings, the application of haptic feedback technology still remains in its infancy. Bridging the gap between haptic technology and the real world to enable ambient haptic feedback on various physical surfaces is a grand challenge in the field of human-computer interaction. This paper presents the concept of an active electronic skin, characterized by three features; richness (multi-modal haptic stimuli), interactivity (bi-directional sensing and actuation capabilities), and invisibility (transparent, ultra-thin, flexible, and stretchable). By deploying this skin on physical surfaces, dynamic and versatile multi-modal haptic display, as well as tactile sensing, can be achieved. The potential applications of this skin include two categories: skin for the physical world (such as intelligent home, intelligent car, and intelligent museum), and skin for the digital world (such as haptic screen, wearable device, and bare-hand device). Furthermore, existing skin-based haptic display technologies including texture, thermal, and vibrotactile feedback are surveyed, as well as multidimensional tactile sensing techniques. By analyzing the gaps between current technologies and the goal of ambient haptics, future research topics are proposed, encompassing fundamental theoretical research on the physiological and psychological perception mechanisms of human skin, spatial-temporal registration among multimodal haptic stimuli, integration between sensing and actuation, and spatial-temporal registration between visual and haptic display. This concept of active electronic skin is promising for advancing the field of ambient haptics, enabling seamless integration of touch into our digital and physical surroundings.

In 1991, Mark Weiser presented the paradigm of ubiquitous computing in Scientific American, emphasizing the profound nature of technologies that seamlessly integrate into daily life until they are imperceptible¹. Ubiquitous computing envisions a world characterized by heightened intelligence and interconnectedness, where the technologies and tools enabling interaction and communication fade into the background, enabling individuals to concentrate on tasks and fostering natural, convenient human-computer interaction.

Over the past three decades, the paradigm of ubiquitous computing has been realized as "ambient visual display" to accommodate human vision channel (as shown in Fig. 1). Screens of varying sizes, including smartphones, laptops, LED walls and billboards, have ushered in an era of ambient visual information that brings us closer to Weiser's blueprint. Esteemed international institutions like IBM, MIT, Microsoft, and BOE have dedicated significant effort to theoretical and technological research, pursuing the realization of this vision. Advancements in materials, technologies, and processes have been instrumental in achieving breakthroughs in visual display technologies.

While visual information provides typical object features (e.g. size, shape, and color), the absence of tactile feedback limits our perception of critical attributes such as texture, temperature, hardness, etc. A comprehensive understanding of natural human-computer interaction reveals that

¹State Key Lab of Virtual Reality Technology and Systems, Beijing, China. ²School of Mechanical Engineering and Automation, Beihang University, Beijing, China. ³Department of Strategic and Advanced Interdisciplinary Research, Peng Cheng Laboratory, Shenzhen, China. ⁴These authors contributed equally: Yuan Guo, Yun Wang, Qianqian Tong. 🖂 e-mail: hapticwang@buaa.edu.cn



Fig. 1 | From ambient visual display to ambient haptic display.

it necessitates not only visual input but also the involvement of the tactile channel. By synergistically combining visual and tactile perception, users can achieve efficient and convenient interaction with physical environments. In some scenarios, the effective addition of the tactile channel might be able to complement visual stimuli, mitigating information overload and reducing cognitive load.

Inspired by the success of "ambient visual display" and the similarity between human visual and haptic channels, one straightforward question is whether we can create a world with "ambient haptic display". In 2009, MacLean introduced the concept of "Ambient Interfaces"², while she proposed the idea of leveraging tactile devices to address attention overload during human-computer interactions. However, haptic technologies remain in their nascent stages when compared to the remarkable capabilities of human touch, and remain significant challenges in faithfully replicating real and natural tactile information. Nowadays, vibration-based devices stand as the most mature haptic rendering technology, extensively employed in commercial devices like smartphones, gaming controllers, and massage chairs, offering information cues, enhanced tactile sensations, and emotional experiences. In research labs, lots of haptic devices, encompassing texture, softness and thermal feedback devices, as well as electronic skins with tactile sensing capabilities, have also been developed. Nonetheless, these devices primarily exist as research prototypes rather than industrial products, often failing to achieve sustained robustness, stability, and reliable tactile feedback. More importantly, these devices are hard to integrate with daily objects and thus fulfill the dream of Mark Weiser ("The most profound technologies are those that disappear. They weave themselves into the fabric of everyday life until they are indistinguishable from it"1). Consequently, the realization of the goal of "ambient haptics" remains elusive.

In this paper, we propose a skin-like interface, i.e., active electronic skin (abbreviated as AE-Skin), to fulfill the goal of "ambient haptics". To meet the demands for ambient haptic interactions, from a form factor perspective, the AE-Skin needs to be thin, transparent, and flexible, allowing convenient attachment to diverse object surfaces without obstructing its functionality. To enable bilateral haptic interactions between users and objects in the surroundings, the AE-Skin perceives user interaction behaviors and seamlessly delivers the required tactile information. In one aspect, it should possess the ability to faithfully reproduce diverse tactile information, encompassing textures, temperatures, vibration, and other physical attributes of various objects. In the other aspect, it should exhibit human-like perception capabilities, dynamically adjusting its output by discerning users' interaction commands such as contact pressure, position, and temperature (as illustrated in Fig. 1). The AE-Skin aims to provide tactile feedback and sense human interaction actions anytime and anywhere, effectively reducing the interaction burden and fostering natural human-computer interaction.

The structure of this paper unfolds as follows: First, we introduce the concept of AE-Skin, and elaborate on its three fundamental characteristics: richness, interactivity, and invisibility. Second, attention is devoted to the two categories of potential applications of the AE-Skin, namely interaction with the physical world (e.g., intelligent home, intelligent car, and intelligent

museum) and interaction with the digital world (e.g., haptic screen, wearable device, and bare-hand device). Third, the state-of-the-art key technologies of AE-Skin are encapsulated, encompassing texture display, temperature rendering, vibration rendering, multidimensional tactile sensing technology, materials and fabrication methods. Fourth, by identifying the gaps between present technologies and the goal of AE-Skin, four prospective research directions are delineated. Finally, we present concluding remarks.

Concept and fundamental features of AE-Skin Concept of AE-Skin

As the primary sensory organ, the human skin covers the whole body and perceives diverse interaction information through mechanoreceptors, such as fabric texture, object temperature, and smartphone vibration. This information is transmitted to the brain, providing a judgment basis for the user's interaction behaviors. During human-object interaction, the user can perceive multiple attributes of objects through the skin, but the object lacks the ability to sense human interaction information. To enable objects to perceive interaction information from humans or other objects in surrounding environments, researchers have pursued the development of electronic skin (e-skin) since the 1970s³. E-skin is an artificial skin with human-like perception capabilities, which can monitor the user's interaction information by endowing interactive devices with remarkable sensing abilities⁴. In order to improve the mechanical properties of the e-skin to accommodate various curvature surfaces, researchers have developed flexible and stretchable e-skin using different sensing principles, enabling the sensing of multidimensional information including temperature, pressure, and strain.

Existing e-skin is limited to the ability of tactile sensing, unable to provide users with tactile feedback, making it impossible to achieve high-fidelity, natural, and bidirectional tactile interaction. The desired interaction mode immerses users in an intelligent interactive space where all objects are touchable. To establish such an intelligent interactive space, it is necessary to develop the next generation of intelligent tactile devices, known as AE-Skin. These devices can be attached to diverse object surfaces effortlessly, enabling the sensing and identification of the user's multidimensional interaction information anytime, anywhere. Additionally, they can provide multimodal tactile feedback, assisting users to perform various interaction tasks more conveniently and naturally. Moreover, the high transparency of AE-Skin is essential in specific interaction scenarios to prevent obstruction of objects, such as displays.

As shown in Fig. 2, the ultra-thin, transparent AE-Skin covers object surfaces. In the interaction process, the AE-Skin dynamically monitors and perceives the contact pressure, interaction position, sliding speed, finger temperature, etc., and the user's interaction intention can be obtained according to these interaction behaviors. The microstructural features, vibration frequency, amplitude, and surface temperature of the AE-Skin can be modulated actively through a closed-loop control system, providing users with rich tactile feedback. The mechanoreceptors in human skin transmit the above tactile information to the brain's central nervous system through ascending nerve channels. Through the processing and recognition of diverse neural cells in the brain, the user can perceive various tactile information from the AE-Skin.

Fundamental features of AE-Skin

To meet diverse interaction requirements in ambient haptic applications, we present three fundamental features of AE-Skin: richness, interactivity, and invisibility (as shown in Fig. 2).

In terms of richness, AE-Skin should possess the sensing ability of multidimensional interaction to identify the user's interaction position, speed, contact force, temperature, etc., and predict the user's interaction intention. In order to accurately and reliably monitor the user's interaction information, it is necessary to consider the sensing range, sensitivity, accuracy, repeatability, temperature excursion, etc. Furthermore, AE-Skin should provide multi-modal tactile feedback, including texture, vibration, and temperature. In practical applications, there are many factors that affect



the efficiency and accuracy of users performing interactive tasks, such as the stability of force feedback, resolution and holding force in texture display, vibration frequency and amplitude of vibration feedback, and temperature range and latency of temperature feedback.

Regarding interactivity, to provide an intelligent, natural, and realistic tactile experience, AE-Skin requires the ability of closed-loop control, which automatically adjusts tactile feedback by identifying the user's interaction information. For example, in an intelligent museum, large-scale AE-Skin can be used to simulate exquisite embroidery in the Tang Dynasty. When visitors touch different positions of the intelligent embroidery, the AE-Skin dynamically displays corresponding texture patterns by precisely controlling actuators in these areas, thus enabling realistic embroidery experiences. Additionally, to meet the spatial registration requirement of the actuators and sensors on the AE-Skin, it is necessary to ensure that the contact area between the fingertip and the AE-Skin covers at least one actuator and one sensor. The spatial layout of actuators and sensors allows the normal sensing and transmission of sensing signals, as well as reliable haptic display. In addition, the update rate of closed-loop control of the actuating and sensing signals should meet the real-time requirements of interactive applications.

For the feature of invisibility, AE-Skin should be as thin as possible, allowing it to hide in the interaction background and transform into an interaction boundary without diverting the user's attention. When detecting the user's interaction, AE-Skin should naturally and progressively perceive and display tactile information, avoiding sudden appearance or disappearance, thus minimizing the user's cognitive load. To be integrated into the interaction environment without obstructing the appearance of objects, AE-Skin should exhibit a certain level of transparency. For example, when an AE-Skin is attached to the surface of the screen, it cannot affect the display of the visual information on the screen. In addition, it should also allow easy and rapid adhesion to various object surfaces, accommodate various curvature surfaces, and enable high freedom of movement for multijoint/soft objects. To adapt to surfaces with different shapes and different physical properties, as well as to ensure high reliability during dynamic action, the range of bending angles and stretchability of the AE-Skin need to be considered.

Killer applications of the AE-Skin Taxonomy of application

The application of AE-Skin can be divided into two main categories based on its ability to adhere to different objects. As shown in Fig. 3, the first category involves applying AE-Skin to the surface of physical objects, such as furniture, automobiles, and exhibits. By infusing these objects with "feelings", AE-Skin brings them to life, enabling the digitization of the physical world. The second category focuses on applying AE-Skin to the surfaces of intelligent devices, including iPads, VR controllers, and haptic gloves. By giving these devices "physical embodiments", AE-Skin facilitates the materialization of the digital world. Both scenarios allow users to interact more naturally and intuitively with everything around them for a more authentic and immersive interactive experience.

Active skin for the physical world

In typical interactive scenarios such as intelligent home, intelligent car, and intelligent museum, AE-Skin can endow objects with tactile sensing and feedback capabilities to realize adaptive adjustments and personalized services possible, providing users with a more intuitive, affinitive, and comfortable interactive experience (as shown in Fig. 3).

Intelligent home: Smart wallpaper affixed with large-scale AE-Skin can alter its micro-surface morphology to present users with textured wall materials such as diatomaceous earth, stone, and ceramic, providing a richer tactile experience (as shown in Fig. 4). Smart tablecloth with medium-sized AE-Skin adjusts automatically its temperature based on seasons and weather conditions, as well as its surface texture patterns according to user preferences and needs. Small-sized AE-Skin can be applied to handheld objects such as doorknobs. When users return home from cold outdoors, the smart doorknob can sense their body temperature and activate the air conditioning in advance. Users can also be notified through vibrations if the door is not properly locked.

Intelligent car: Steering wheel integrated with AE-Skin makes it possible to naturally monitor drivers' physiological and behavioral parameters such as hand pressure and grip position. In cases of non-compliant or fatigued driving, the smart steering wheel activates vibration warnings. AE-Skin can also be affixed to the surface of car panels (e.g. instrument panels and car doors), transforming physical buttons into intelligent ones. When the driver touches the buttons while driving, the AE-Skin provides continuous tactile guidance, ensuring the accuracy of their actions, as well as notifying the completion of the operation (as shown in Fig. 5). Current tactile devices can only realize a single function (sensing or feedback), and cannot simultaneously record the driver's interactive information and provide tactile feedback for drivers⁵⁻⁹. For example, Luo et al.⁸ adopt the pressure signals obtained from piezoelectric sensors embedded in the carpet to tracking of the driver's posture. Kim et al.⁶ have designed a soft vibrotactile interface to remind the driver of the vehicle's navigation information. In terms of interior design, AE-Skin can simulate tactile sensations of different textures, providing designers with a more realistic and intuitive sensory experience when selecting materials. Additionally, designers can fine-tune simulated texture patterns (e.g., groove depth and spacing) using texture presentation devices based on application scenarios and customer needs. This design approach significantly shortens the design cycle, reduces product design and manufacturing costs, and improves product quality and user experience.

Intelligent museum: AE-Skin can enhance the vitality and authenticity of exhibits with dynamic patterns and temperature feedback, offering



Fig. 3 | The potential applications of AE-Skin.





immersive and interactive experiences, such as smart books for exhibiting natural phenomena. For example, visitors can feel the temperature changes of heat exchanges, and the frictional sensation of objects sliding on surfaces with different morphological features by touching the AE-Skin. Compared to conventional video displays, tactile feedback of AE-Skin provides a more intuitive approach to presenting scientific knowledge, which could effectively stimulate the exploration interest and curiosity of younger generations. Furthermore, AE-Skin can be used to generate twin replicas of highvalue and fragile artifacts. By digitizing the texture information of ancient inscriptions, engravings, or fabrics, and simulating their morphological features, visitors can touch and feel the artifacts in detail without damaging the original ones (as shown in Fig. 6). Exhibitions enhanced with tactile interactions encourage visitors to actively participate in the learning experience of related historical and cultural knowledge, improving their overall engagement and satisfaction levels.

Active skin for the digital world

Unlike the physical world, digital devices possess limited tangible manipulation. Screens, as the most commonly-used digital interfaces, represent the 2D or 2.5D digital world, while VR devices extend the interaction space to 3D environments with different fixation options. In this section, haptic screens, wearable VR devices, and bare-hand VR devices are highlighted as examples, for describing the materialization of the digital world (as shown in Fig. 3). By applying AE-Skin to the above devices, the integration of sensing and driving capabilities enables closed-loop control of the different tasks and procedures, providing users with a more intelligent and efficient interactive experience.

Haptic Screen: Screens of various sizes have achieved a high level of ubiquity (e.g., smartphones, iPads, televisions, in-car displays, laptops, and advertising screens), presenting a wide range of information and greatly facilitating people's daily lives and work (as shown in Fig. 7). AE-Skin



Fig. 5 | **AE-Skin for intelligent cars.** AE-Skin mounted on car panels can be used to control audio, wind speed, temperature, seat position and seat angle. In the initial state, the panel surface remains flat. When the driver touches the panel, the integrated sensor captures the pressure of the finger, and then the actuator generates a

certain trajectory for interactive guidance. Under the guidance, the driver can be quickly and accurately moved to the specified position and press the designated position for auxiliary operation, while the actuator vibrates to remind the driver whether the operation is correct.



Fig. 6 | AE-Skin for intelligent museums. AE-Skin can be conformally attached on the replica surface, dynamically simulating the texture information of ancient inscriptions, engravings or fabrics. With AE-Skin and VR glass, visitors can touch and see the artifacts in detail without damaging the original ones.



Fig. 7 | AE-Skin for haptic screens. The transparent AE-Skin can overlay the surface of the screen and display the same actual terrain features as the physical keyboard, enhancing the user's interactive experience.



provides the possibility to integrate the rich tactile experience into screens. For example, when attached to the surface of a phone-sized or pad-sized touchscreen, AE-Skin can render the tactile sensation of fabrics (i.e., texture and temperature), enabling users to have a tangible shopping experience with more comprehensive product information or simulate the outline of the clicked item on the screen, optimizing the accuracy and precision of users' finger control (fat finger problem). Especially in in-car displays, tactile guidance allows the driver to perform operations with minimal or no visual input. Furthermore, benefiting from the integrated driving-sensing capabilities of the AE-Skin, product designers can achieve remote collaborative design activities in large-sized touchscreens, such as the manipulation of different materials and forms. However, the currently available screens are limited in their ability to provide multi-modal tactile feedback, as they are only capable of representing a single tactile modal¹⁰⁻¹². Based on the electrostatic adhesion or mechanical vibration, these screens can represent diverse textures to simulate the fabrics with different weaving processes and patterns. For instance, Nai et al.¹² study the use of periodic vibrotactile feedback to represent the patterned textures.

Wearable VR Devices: In interactive virtual environments, existing force feedback gloves attached with AE-Skin make it possible to simulate tactile sensations when a user touches various virtual surfaces such as sofas, tables, and walls, as well as thermal sensations of hot or cold drinks, greatly improving the realism of virtual experiences. Nevertheless, most force feedback gloves provide vibration feedback to the fingertips by integrating with different actuators, such as pneumatic actuators, motors, and piezo actuators. Currently, there is still a lack of force feedback gloves that can provide multi-modal and high spatial resolution tactile feedback^{13–15}. Smart vests with AE-Skin can dynamically adjust their thermal condition based on the user's body temperature and the virtual environment, as well as provide users with embodied navigation and different physical contact. AE-Skin can even be integrated into shoe pads, simulating vibrotactile experiences of walking on grass, sand, mud, or other terrains.

Bare-Hand VR Devices: In recent years, researchers have developed a variety of handheld VR controllers with multiple capabilities that can render different tactile modals (e.g. shape, texture, size, and stiffness) when users interact with virtual objects¹⁶⁻¹⁸. For example, Sun et al.¹⁷ propose a handheld device for bare-hand interactions in the virtual environment, which can render three object properties, namely, size, shape and stiffness. However, the lack of sensors makes it difficult for these VR controllers to detect and distinguish the interactive multi-finger synergistic gestures. AE-Skinaugmented VR controllers can offer enhanced virtual combat experiences

by predicting users' psychological status based on their tactile information such as grip pressure and palm temperature. Increasing grip pressure might indicate a higher combat engagement level. Moreover, by integrating AE-Skin with shape-rendering devices, users can experience virtual objects by touching the digital clay¹⁹ directly using bare hands. However, due to limited operational space, this approach is not suitable for extensive VR interactions. Therefore, AE-Skin can be attached to a mobile platform equipped with digital clay, allowing it to move with the user and render different shapes, temperatures, textures, and vibrations in real-time, and to achieve a more immersive closed-loop control between user perception and object display.

Key technology of the AE-Skin

To meet the application demands of ambient haptic interactions between users and the physical or digital world, AE-Skin needs to display multimodal haptic stimuli and scene users' interaction intention. In recent years, numerous researchers have focused on these objectives and have developed texture display devices, temperature rendering devices, vibration rendering devices, and multidimensional tactile sensing devices based on various materials and fabrication methods. In this section, we will provide a detailed overview of the research advancements in these areas.

To develop a high-fidelity AE-Skin with three fundamental characteristics, several key technologies must be taken into consideration, including multi-modal haptic display, multi-dimensional tactile sensing, materials, and fabrication methods (as shown in Fig. 8). During the design of AE-Skin, the required tactile modalities (e.g. texture, temperature, and vibration) and sensing signals (e.g. pressure, strain, and temperature) are selected based on the interactive scenarios. For a certain selected tactile stimuli or sensing signal, the appropriate materials (e.g. responsive material, and nanomaterial) and fabrication methods (e.g. molding process, soft lithography, and 3D printing) are adopted to prepare the corresponding actuator or sensor. With the use of the aforementioned technologies, the designed tactile device can provide users with an immersive interaction experience. Nonetheless, there are still some challenges that need to be overcome in the future, which will be described in the following section.

Texture display technology for AE-Skin

Texture perception mechanism. The texture is composed of different geometrical features (bumps and grooves) on the surface of an object. Depending on the scale of these features, textures can be categorized into



Fig. 9 | Examples of the texture display device. a Texture display method based on a single-layer electro-active polymer actuator. Reproduced with permission²⁹. Copyright 2015, Springer Nature. b Texture display method based on a multi-layer amplified electro-active polymer actuator. Reproduced with permission³⁴. Copyright 2018, IEEE. c Texture display method based on a hydraulically amplified self-healing electrostatic actuator. Reproduced with permission³⁰. Copyright 2020, John Wiley & Sons. d Texture display methods based on a rigid magnetic actuator. Reproduced with permission⁵². Copyright 2017, IEEE. e Texture display method based on a rigid magnetic actuator and flexible base. Reproduced with permission⁶⁸. Copyright 2016, Springer Nature. f Texture display method based on a soft magnetic actuator. Reproduced with permission⁵⁵. Copyright 2022, IEEE. g Texture display methods

based on shape memory alloy actuator. Reproduced with permission⁷⁹. Copyright 2013, Elsevier. **h** Texture display method based on shape memory polymer actuator. Reproduced with permission⁸⁵. Copyright 2017, John Wiley and Sons. **i** Texture display method based on commercial valves. Reproduced with permission⁹³. Copyright 2012, IEEE. **j** Texture display method based on microvalves. Reproduced with permission¹⁰¹. Copyright 2014, Royal Society of Chemistry. **k** Texture display method based on chemical combustion. Reproduced with permission¹⁰². Copyright 2021, National Academy of Sciences. **I** Texture display method based on liquid crystal elastomer actuators. Reproduced with permission¹⁰⁴. Copyright 2014, Elsevier. **m** Texture display method based on artificial muscle actuators. Reproduced with permission¹⁰⁵. Copyright 2019, John Wiley & Sons.

millimeter-level features and micrometer-level features. The boundary value of the scale is reported to be about 1 mm²⁰. The combination of texture features at different scales forms specific texture patterns. Katz proposed the "Duplex Theory" of texture perception, perception of texture depends on two cues, i.e. spatial cues and temporal cues. Spatial cues are determined by the size, shape, and distribution of surface elements. Temporal cues are determined by the rate of vibration as skin is moved across finely textured surfaces. Research has shown that during the process of touching millimeter-level texture features, the SAI receptors within the skin are activated to encode the spatial patterns of the texture features²¹. In contrast, touching micrometer-level texture features induces high-frequency vibrations in the skin, activating the PA and PC receptors, which encode the vibration information of millimeter-level texture features into temporal peak patterns²¹. These encoded signals are transmitted through the ascending neural pathways to the perception

area of the brain cortex, where they are further decoded and processed to identify different texture information.

Based on the different approaches to presenting texture information, existing texture display technologies can be divided into two categories. The first category is sensory substitution (for simulating micrometer-level texture features), which involves non-morphological changes to present texture information. Different methods, such as electrostatic adhesion, ultrasound, and mechanical vibration, are used to adjust the normal or tangential force between users' fingers and the surface of the device to render different texture information. For detailed studies on non-morphological texture display methods, please refer to previous review papers²².

The second category is the faithful reproduction of object surface morphology (for simulating millimeter-level texture features), achieved by creating variable microstructures on the device surface using specific mechanical structures and actuation mechanisms. Users can perceive

https://doi.org	/10.1038/	s41528-02	4-00311-5
-----------------	-----------	-----------	-----------

Table 1 Summary	/ of performance	of represents	ative texture di	splay d	evices re	ported in the lit	erature						
Actuation principle	Actuating material	Diameter of actuator	Spatial resolution	Array	Holding force	Vertical displacement	Response time	Flexibility	Stretchability	Thickness	Transparency	Consumption	Ref.
Electro-active material	HAXEL	6 mm	6 mm	5*5	>300mN	0.5 mm	<5 ms	٢	Ν	0.8 mm	Ν	34 W.kg ⁻¹	30
	Multi-layer EAP	2 mm	3 mm	10*10	>20mN	1.8 mm	100 ms	٢	Z	0.4 mm	Z	/	33
Electromagnetic actuation	Coil + soft magnetic actuator	1.5 mm	3 mm	5*5	/	0.65 mm	530 ms	×	×	/	Z	59.15mJ	56
	Coil + permanent magnet	1.5 mm	2.5 mm	16*12	>30 N	0.6 mm	5 ms	z	Z	5.5 mm	Z	1 W	61
Thermal actuation	SMA	1.5 mm	2.5 mm	5*2	196mN	0.8 mm	500 ms	z	Z	30 mm	Z	1.331 W	72
	SMA	1.5 mm	2.6 mm	8*8	300mN	1 mm	1.5 Hz	z	N	50 mm	Ν	176 mW	77
	SMP	3 mm	4 mm	32*24	1.5 N	0.25 mm	2.5 s	Z	Ν	2 mm	Ν	/	85
Pneumatic actuation	Bubble actuators	7.5 mm	13mm-14mm	2*3	1.5 N	3 mm	/	٢	٢	2.5 mm	٢	27.6kPa	88
	Exothermic reaction	/	/	3*3	/	6 mm	1 ms	٢	٢	/	٢	3 W	102
Optical actuator	LCE	0.8 mm	2.5 mm	10*10	40 mN	1.3 mm	>3 s	Z	Ν	30 mm	Ν	0.3 W	104
artificial muscle actuator	TSAM	8 mm	12 mm	5*5	<10 mN	0.45 mm	4 S	~	Y	3.2 mm	z	2 V	105

simulated texture patterns by touching the actuated microstructures. According to the different actuation principles, these methods mainly include dielectric-driven, electromagnetic-driven, shape memory-driven, pneumatic-driven, and optically-driven texture display methods. This paper focuses on exploring morphology-based texture display methods. Next, we will introduce the working principles and characteristics of each actuation method. The details of some representative texture display devices are presented in Fig. 9 and Table 1.

Electro-active material based texture display method. Electro-active polymer (EAP) undergoes shape or size changes when subjected to external electrical stimulation (voltage or current)^{23–25}. Based on this working principle, EAP is sandwiched between upper and lower flexible electrodes to form a sandwich structure. Under the external electric field, the electrostatic force generated between the upper and lower flexible electrodes compresses EAP to produce deformation^{26,27}. To generate vertical deformation for texture display, a boundary constraint layer is typically prepared in the circumferential direction of the EAP actuator, which converts in-plane deformation into out-of-plane deformation, thus forming micro-scale surface morphology changes on the texture display device^{28,29}.

The EAP-based texture display method has a high response frequency, which can meet the real-time interaction requirements for haptic feedback. However, this method faces challenges of limited vertical deformation and low holding force³⁰⁻³². To address these issues, a multi-layer EAP actuator is stacked vertically to increase the vertical displacement and holding force of the texture display devices^{33,54}. In addition, EAP actuators require high driving voltage (several thousand volts), which poses a certain safety risk³⁵. To improve interaction safety, a flexible insulating film is typically applied to the surface of the EAP actuator to protect users from high-voltage shocks³⁴. In recent years, some researchers have developed dielectric elastomer materials with high dielectric constants, which are promising alternatives for reducing the driving voltage to hundreds of volts, improving the safety of the texture display device³⁶⁻³⁸.

Different from the multi-layer superposition amplification method, the hydraulically amplified self-healing electrostatic (HASEL) actuator exploits the combination of hydraulic and electrostatic forces to realize the amplification of the holding force and vertical displacement^{30,39}. HASEL actuators employ liquid as the dielectric layer instead of elastomers, and the dielectric fluid is encapsulated within a sealed chamber formed by upper and lower electrostatic force compresses the liquid to achieve high-speed electrohydraulic actuation, forming bumps on the surface of the tactile device. Compared to EAP actuators, HASEL actuators exhibit more stable characteristics and effectively avoid potential dielectric breakdown⁴⁰, but the challenges of fluid encapsulation and actuator miniaturization remain to be addressed.

Electromagnetic-actuated texture display method. Electromagnetic actuators have the advantages of fast response, simple structure and stable performance, and have been widely applied in soft robotics⁴¹⁻⁴³ and texture display devices⁴⁴⁻⁴⁷. Under the exciting magnetic field generated by the electromagnetic coil or solenoid, the permanent magnet moves upward (named as the raised solution) and forms bumps on the device surface, and the bumps at different positions form a certain texture pattern⁴⁸⁻⁵⁴. In the raised solution, the electromagnetic force is also used to provide a holding force to resist the finger's pressure during the interaction. To provide sufficient holding force, it is necessary to increase the drive current or the size of the electromagnetic coil, which will reduce the spatial resolution of the texture display device. A promising alternative is to adopt a sunken solution, in which a groove rather bump is formulated to generate geometric profiles encoded in the target texture pattern^{55,56}. In the sunken solution, the holding force is provided by the base of the texture display device, and the electromagnetic force is solely used to create the grooves, which significantly reduces the demand for

electromagnetic force and effectively improves the spatial resolution of the device.

In electromagnetic-actuated texture display devices, the magnetic interference between adjacent electromagnetic coils will reduce the stability of the device and seriously affect the user's interactive experience. To address this challenge, a shielding layer is commonly employed to envelop each electromagnetic coil to change the magnetic flux distribution, thereby reducing the magnetic interference between electromagnetic coils^{52,56–58}. In addition, the electromagnetic-actuated texture display devices require numerous electromagnetic coils to keep continuously working to maintain a certain pattern. A long period of working will not only increase energy consumption, but also result in high temperatures and even burnout of the electromagnetic coil, affecting the user experience. The latch structure is employed to lock the moving position of the magnetic actuators, which can realize the preservation of the texture pattern without energy consumption^{59,60}. According to the latch principle, the existing latch mechanism can be categorized into mechanical structure-based latch method⁶¹⁻⁶⁴ and electromagnetic force-based latch method^{56,65,66}.

Most existing electromagnetic-actuated texture display devices consist of rigid electromagnetic coils, permanent magnets, and rigid bases, and the rigid components and structures cannot be attached to surfaces of objects with different curvatures, failing to meet the requirements of flexible and stretchable AE-Skin. A simple and effective solution is to embed rigid electromagnetic coils and permanent magnets into flexible substrate materials, which feature with small bending angle and lower stretchability^{67,68}. At a larger bending angle, the rigid components will be separated from the flexible substrate. Wang et al.,55 developed a soft texture display device, which consists of soft magnetic units and a soft membrane bracket. Under the external magnetic field generated by the rigid electromagnetic coil, the magnetic units sink to form pits and represent a desired texture pattern. To achieve flexibility in electromagnetic coils, an effective solution is to encapsulate liquid alloy in a flexible silicone tube as a substitute for rigid electromagnetic coils⁶⁹⁻⁷¹. Compared to rigid electromagnetic coils, flexible electromagnetic coils have higher resistance, which requires a larger excitation current to generate the same electromagnetic field. Additionally, the size of the flexible electromagnetic coil based on the above fabrication process is relatively large, and the miniaturization technology of the flexible electromagnetic coil needs to be explored to meet the spatial resolution requirements of texture display devices.

Shape memory actuator-based texture display method. Compared with traditional actuators, shape memory actuators possess characteristics such as high strain, large power-to-weight ratio, and simple driving mechanism, making them extensively utilized in texture display devices^{72–74}. Most shape memory actuators belong to thermally driven materials. When the temperature reaches the phase transition temperature, the shape memory alloy (SMA) actuator contracts in length, which causes the pin to move upward, forming a bump of 2.6-mm height on the surface of the device⁷⁵. As the temperature decreases below the phase transition temperature, the SMA actuator gradually recovers to its original length, and the pin gradually descends. Thanks to the simple driving mechanism and structural layout, the spatial resolution of the device can reach 2 mm⁷⁶.

During the interaction, SMA actuators need to be energized for an extended period to maintain the raised state of the pin, which may lead to a rapid increase in the surface temperature of the texture display device, affecting the interaction experience. The surface temperature can be partially reduced by installing fans, and heat sinks⁷⁷, but the cooling effect is limited. To avoid prolonged energization, an effective solution is to install the magnetic components on the pin and the base respectively, and lock the position of the pin with electromagnetic force^{78–81}. When the pin reaches the top position under the action of the SMA actuator, the magnetic component on the pin is attracted to the magnetic component on the base. The resulting electromagnetic force enables the pin to maintain the protrusion state even after the SMA actuator is not continuously activated.

In recent years, shape memory polymer (SMP) actuators have garnered more attention as promising actuators for texture display devices because of their flexibility and excellent mechanical performance^{82,83}. Within a narrow temperature range, Young's modulus of SMP can be regulated by several orders of magnitude⁸⁴. Benefiting from the controllable and reversible stiffness, some researchers developed a texture display device with the latch function. By patterning an array of miniature stretchable heaters on SMP actuators, one single pneumatic supply is adopted to rapidly and selectively reconfigure any or all elements^{85–87}. When the heater is powered on, Young's modulus of the SMP actuators is reduced by >100-fold variation. Under positive/negative pressure, the SMP actuator deforms and produces bumps/ grooves. The heater is turned off and the pressure is kept on to latch the morphological change in place as the SMP actuator cools, which takes ~2.5 s⁸⁵. Subsequently, the pressure is switched off, the device can achieve the preservation of the bumps/grooves without energy consumption.

Pneumatic-actuated texture display method. Pneumatic actuators have gained favor among researchers due to their wide range of power sources, low cost, and simple structure, and they are widely applied in texture display devices and wearable devices^{88,89}. Under positive pressure, the pin in the pneumatic chamber moves upward^{90–92} or the soft membrane on the device surface deforms^{88,93} to form the bump. The height of the bumps and the holding force depends on the value of the air pressure. By regulating the air pressure of different tactile units, the pneumatic-actuated texture display device can achieve a dynamic presentation of different texture patterns. To achieve independent control of the tactile units, each tactile unit requires a separate valve to control the on-off of the air pressure. The number of the values increases with the number of tactile units, and the increased cost and volume of the control system restrict the promotion and application of large-area pneumatic-actuated texture display devices.

In recent years, microfluidic systems based on soft lithography techniques have attracted wide attention due to their high integration, small size, precise control, and low fabrication cost⁹⁴⁻⁹⁶. With the development and progress of this technology, microvalves with different functionalities (e.g. multiplexing, pressure regulation, and flow control) have been developed^{97–100}, providing a feasible solution for miniaturization and cost reduction of pneumatic-actuated texture display devices. By adjusting the open/closed states of microvalves, the surface morphological features of the texture display device can be switched to represent a certain texture pattern^{89,101}. In addition to the valves, the bulky pump also limits the miniaturization and portability of pneumatic-actuated texture display devices. Heisser et al.¹⁰² have proposed a promising solution that utilizes the exothermic reaction of methane combustion to achieve the deformation of the tactile unit. This method has the advantages of high response frequency (1 kHz), large deformation displacement (6 mm), and low power consumption (3 W), but it cannot provide a continuous and stable air source for the texture display devices.

Other methods for texture display. In addition to the abovementioned several actuation principles, liquid crystal elastomer (LCE) actuators and artificial muscle actuators can also be used on texture display devices. LCE materials can undergo reversible contraction and expansion in response to an applied light. Based on this characteristic, Camargo et al.¹⁰³ prepared the LCE actuator into a bulging shape. When the light source turns on, the raised LCE actuators contract, and the surface of the texture display device changes from a raised state to a smooth state. Based on the same driving principle, the LCE actuator is fixed at the bottom of the pin, and the pin is pushed upward to form a bump on the device surface through the contraction of the LCE actuators¹⁰⁴. LCE actuator-based texture display devices have the advantages of low power consumption and simple structure, but suffer from limitations such as low response frequency and low holding force.

Inspired by the cephalopods papillae, Lamuta et al.¹⁰⁵ developed a texture display device based on artificial muscle actuators. The artificial



Fig. 10 | Examples of the temperature display device. a Temperature rendering device based on rigid Peltier patch. Reproduced with permission¹³³. Copyright 2019, Springer Nature. **b** Temperature rendering device based on flexible Peltier patch. Reproduced with permission¹¹⁶. Copyright 2020, John Wiley & Sons. **c** Temperature

rendering device based on thermal resistance heating principle. Reproduced with permission¹³⁷. Copyright 2016, American Chemical Society. **d** Electronic skin based on thermal resistance heating and hydrogel cooling principle. Reproduced with permission¹⁴⁴. Copyright 2023, National Academy of Sciences.

muscle actuator is composed of nylon wires and metal heating wires. At a 2-V voltage, the metal wire heats the artificial muscle actuator to produce the reversible deformation, forming a 0.45-mm bump on a device surface. The artificial muscle actuator-based texture display device has the advantages of low power consumption and simple structure, but it is unsuitable for high spatial resolution and dynamic texture display devices due to the limitation of the size and response frequency of the artificial muscle actuator.

Temperature rendering technology for AE-Skin

Temperature perception mechanisms. In 2021, the Nobel Prize in Physiology or Medicine was awarded to David Julius and Arden Patapoutian. They utilized capsaicin to identify receptors in the peripheral nerves of the skin that respond to heat, laying the groundwork for the discovery of other temperature receptors. Cold sensation and warmth sensation, collectively known as thermal sense or temperature sense, reveal the biophysical mechanisms of neural signal induction in response to different temperatures, advancing our understanding of the perception of cold and hot stimuli¹⁰⁶.

The perception of temperature in the human body is associated with the type of stimulus, whether it is cold or hot. Research has shown that the conduction velocity of afferent fibers in cold receptors (typically ranging from 10 to 20 m/s) is higher than that in heat receptors (typically ranging from 1 to 2 m/s)¹⁰⁷. Consequently, the body responds faster to cold stimuli compared to hot stimuli. Furthermore, the temperature perception in the human body is influenced by factors such as the baseline temperature of the skin, the temperature of the stimulus/environment, the location of the stimulated skin, and the rate of temperature change¹⁰⁸⁻¹¹². In an environment ranging from 25 to 40 °C, a higher baseline skin temperature results in a lower threshold for warmth perception, whereas a lower baseline skin temperature leads to a lower threshold for cold perception. In an environment ranging from 30 to 36 °C, where both types of receptors are simultaneously firing, the human skin does not perceive the variation in temperatures¹¹³. Cold receptors are activated within the range of 15 to ~30 °C, while heat receptors are activated within the range of 36-45 °C, allowing individuals to distinctly perceive temperature changes^{113,114}. When the temperature exceeds 45 °C or falls below 15 °C, pain receptors are activated, causing a sensation of pain^{114,115}. Therefore, it is essential to control the output temperature of the AE-Skin within the range of 15-45 °C to avoid potential injure to the human body^{113,116}.

Temperature rendering methods. Temperature rendering devices achieve thermal exchange between the human skin and the device through physical contact, providing users with a tactile experience of different temperatures. They are widely applied in virtual reality^{117,118}, augmented reality^{119,120}, human-computer interaction^{121–123}, and other fields. Based on different working principles, existing temperature rendering devices can be classified into two main categories: Peltier elements^{124–126} and thermo-resistive heaters^{127–129}. The details of some representative temperature rendering devices are presented in Fig. 10 and Table 2.

In the design of temperature rendering devices, the first consideration is flexibility and stretchability to ensure that the device fits well on the human skin surface^{113,130}, providing users with effective temperature feedback and reducing heat dissipation during the conduction and interaction. Secondly, temperature rendering devices need to have a fast response speed to meet the requirements of interaction scenarios with significant temperature differences¹³¹. For example, when simulating the feeling of touching hot coffee on a cold winter day, the temperature rendering device needs to first provide a cold sensation to simulate the winter chill and then quickly increase the temperature to simulate the warmth of hot coffee. Additionally, the temperature adjustment process needs to be dynamically controllable to minimize the temperature fluctuations and ensure that the temperature rendering range will not cause harm to humans (exceeding 45 °C or falling below 15 °C)^{113,116,131}.

Peltier devices consist of N/P-type semiconductors, electrodes, and substrates. Under an external excitation current, charged carriers move from one semiconductor to another semiconductor, resulting in the release or absorption of heat¹³². Based on this principle (thermoelectric effect), Peltier devices can directly transfer thermal energy using electrical energy to achieve cooling or heating and stimulate the user's thermal receptors. By adjusting the magnitude and direction of the excitation current, precise control of heating/cooling temperature and heating/cooling direction can be achieved. To increase the temperature range and adjustment speed, a fan/ cooling tablet is used to accelerate heat dissipation on the heating side to achieve better interactive effects¹³³. Commercial Peltier devices typically have N-type and P-type semiconductors that are usually fixed on rigid substrates^{118,133,134}. However, rigid Peltier devices cannot conform to the surface of the human skin, reducing the interaction area between the skin and the device and weakening the cooling/heating effect. To address this

Table 2 Summar	y of performance of re	presentative ten	nperature display d	evices reported in t	he literature			
Actuation principle	Actuating material	Actuator size	Temperature range	Cooling or heating	Response time	Consumption	Flexibility	Ref.
Peltier effect	Rigid Peltier device	1	12 °C-45 °C	Cooling and heating	~1.0 °C s $^{-1}$ for heating and 1.0 °C s $^{-1}$ for cooling	1.5 A	Y	116
	Flexible Peltier device	5 mm * 5 mm	/	Cooling and heating	/	123.74uW	¥	135
	Flexible Peltier device		0°C-68.5°C	Cooling and heating	~24.85 °C s $^{-1}$ for heating 10.85 °C s $^{-1}$ for cooling	18.5 W	٨	136
Thermo-resistive	Metal nanowires	1	25°C-180°C	Heating	~2.0 °C s $^{-1}$ for heating	. 1	≻	137
	Resistance and Hydrogel	14.4 mm * 14.4 mm	27°C-40°C	Cooling and heating	~1.86 °C s $^{-1}$ from 27 °C to 40 °C	0.5 W	¥	144
	Metal nanofibers	24 mm * 32 mm	25°C-250°C	Heating	~0.76 °C s $^{-1}$ for heating from 29 °C to 42 °C	$0.65~\mathrm{W}~\mathrm{cm}^{-2}$	٢	319
	Liquid alloy	1	25°C-83.24°C	Heating	~0.77 $^\circ\text{C}$ s $^{-1}$ for heating from 25 $^\circ\text{C}$ to 83.24 $^\circ\text{C}$	1 W	Y	320

Review article

issue, an effective solution is to fix rigid P/N-type semiconductors on flexible substrates^{135,136}, utilizing the flexibility of the substrate to enable better attachment of the temperature-rendering device to the skin surface, thus enhancing the user's interactive experience.

The working principle of thermo-resistive heaters is based on Joule's law, where the generated heat is related to the resistance, current, and heating time. By adjusting the applied current/voltage, the surface temperature of the thermo-resistive heater can be precisely controlled. Moreover, this method can deliver a large amount of heat to the skin, achieving and maintaining a high output temperature¹³¹. With the continuous development and progress of materials and technologies, a large number of conductive materials have been developed, such as metal nanowires^{137,138}, carbon nanomaterials^{139,140}, and conductive polymers¹⁴¹. The flexibility of thermo-resistive heaters has been realized by embedding conductive materials into an elastic matrix. Additionally, some researchers have employed structures such as serpentine-mesh structures¹⁴², wrinkled structures¹⁴⁰, and weaving structures¹⁴³ to achieve the flexibility and stretchability of thermo-resistive heaters. Compared to Peltier devices, thermo-resistive heaters cannot provide cooling feedback to users during the interaction process. To address this issue, Rogers et al.¹⁴⁴ proposed a closed-loop temperature control device, which consists of a thermo-resistive heater based on a copper wire serpentine mesh structure, a passive cooling hydrogel, and an actively switched thermal barrier interface. In the cooling mode, the hydrogel efficiently couples heat with the thin thermal barrier interface, and the evaporation of moisture in the hydrogel lowers the surface temperature of the skin, providing a cold sensation to the user (27 °C). In the heating mode, the heat generated by the thermo-resistive heater causes the liquid inside the thermal barrier interface to undergo a phase change from liquid to vapor. This results in an expansion of the thermal barrier interface and isolates the hydrogel from the heater, effectively reducing heat dissipation from the heater and enabling the heater to reach 35 °C within 5 s.

Vibration rendering technology for AE-Skin

Vibration perception mechanism. The human skin is highly sensitive to vibration stimuli, and even weak mechanical vibrations can activate superficial tactile receptors, enabling individuals to perceive vibrotactile information. The perception process of vibrotactile information by receptors involves transduction and vibration encoding. When mechanoreceptors are stimulated by mechanical vibrations, they convert the vibration signals into action potentials through transduction. Simultaneously, the receptors encode the vibration information, such as vibration amplitude, frequency, and duration, into sequences of action potentials. The encoded action potentials are then transmitted through the ascending neural pathway to the cerebral cortex, enabling the perception of vibration signals¹⁴⁵.

The density of mechanoreceptors varies across different body parts¹⁴⁶. For example, in hairless skin areas such as the hands and feet, both Pacinian and Meissner corpuscles exhibit high densities, making it easier to perceive vibration stimuli^{146,147}. However, in areas with hairy skin, the spatial density of Pacinian corpuscles significantly decreases, and Meissner corpuscles are completely absent^{148,149}. Furthermore, each type of mechanoreceptor has a different perceptual range. Meissner corpuscles are sensitive to relatively high-frequency skin deformation^{150,151} and have a frequency perception range of 5-50 Hz vibration^{146,152}. On the other hand, Pacinian corpuscles respond to a wider range of high-frequency vibrations and can perceive transient interactive information^{153,154}, with a frequency perception range of 40–400 Hz vibration 146,152 . Additionally, when a vibration rendering device provides vibrotactile feedback to the user, it is essential to consider whether the presented vibration information can be perceived by the user. In psychophysical experiments, the absolute detection threshold and the relative discrimination threshold are often used to represent the perceptual ability of the human body in relation to external stimuli^{155,156}. The sensory detection threshold for a particular individual depends on various factors, including the vibration display device, testing procedure (e.g. vibration frequency, amplitude, and stimulus location), subject's characteristics (e.g. age, gender,



Fig. 11 | Examples of vibration feedback devices. a Tactile belt based on rigid vibration motor. Reproduced with permission¹⁷². Copyright 2011, IEEE. **b** Electronic skin based on flexible vibration motor. Reproduced with permission¹⁷⁶. Copyright

2019, Springer Nature. **c** Vibrotactile device based on the dielectric actuator. Reproduced with permission¹⁸⁶. Copyright 2021, John Wiley & Sons. **d** pneumatic actuator. Reproduced with permission¹⁷⁹. Copyright 2021, John Wiley & Sons.

Actuation principle	Actuator size	Spatial resolution	Array	Vibration frequency	Vibration amplitude	Output force	Flexibility	Stretchability	Thickness	Consumption	Ref
Electromagnetic	18 mm diameter	21 mm	6*6	300 Hz	280um	135 mN	Y	Y	2.5 mm	1.75 mW/14 W	176
	3 mm * 3 mm	14 mm	4*4	200 Hz	200um	12.1mN	Y	Y	4.2 mm	115 mW	178
	5 mm diameter	/	1*5	250 Hz	300um	/	Y	Y	5.8 mm	150 mW	177
Pneumatic	10 mm diameter	/	1*1	100 Hz	3.2 mm	1 N	Y	Y	500um	40kPa	182
	8 mm diameter	/	1*1	90 Hz	300um	0.3 N	Y	Y	900um	/	179
DEA	3 mm * 15 mm	/	1*1	1–500 Hz	6um	9mN	Y	Y	18um	450 V	186
	2 mm diameter	/	10*10	200 Hz	1.8 mm	21 mN	Y	N	400um	3000 V	187

Table 3 | Summary of performance of representative vibration display devices reported in the literature

skin temperature, and stratum corneum thickness), and psychophysical testing protocols. Further comprehensive and in-depth reviews on this topic are available in the references^{157,158}.

Vibration presentation techniques. Mechanical vibration stimulation, as the most mature tactile feedback technology, is widely used in various aspects of our daily lives, such as rendering object properties, perceiving interactive positions, and conveying abstract information. During the interaction between humans and objects, mechanoreceptors perceive a significant amount of vibration information, and the surface properties of objects can be recognized by processing and analyzing these vibration signals. Based on this characteristic, vibrational stimuli applied to the contact surface can be used to modulate the perception of texture roughness¹⁵⁹ and friction sensation¹⁶⁰, thus rendering different surface properties of objects. Additionally, some researchers have employed the arrangement of vibration actuators on different parts of the body to simulate the perception of interactive positions. For example, in virtual military training, vibration stimulation is utilized to simulate the collision between a soldier's body and virtual objects to enhance the soldier's situational awareness of interactive scenarios¹⁶¹. In the realm of gaming and entertainment, the vibration actuators on various body parts are used to simulate different attack positions, greatly enhancing the interactivity and immersion of the game. In terms of conveying abstract information, vibration stimulation can be used for tactile communication for visually impaired people^{162,163}, navigation aids^{164,165}, emotional transmission¹⁶⁶, and vehicle warning^{167,168}. The details of some representative vibration rendering devices are presented in Fig. 11 and Table 3.

Mechanical vibration stimuli are applied directly to the human skin and are typically implemented through back-and-forth motion perpendicular to the skin surface^{155,169}. The most traditional way is to use electromagnetic-based motors to provide vibration feedback. Over the past few decades, many researchers have developed various tactile devices based on rigid motors to provide users with tactile feedback, such as vibration jackets^{170,171}, vibration belts^{172,173}, and vibration gloves^{174,175}. To ensure a satisfactory interaction experience, it is often necessary to use tapes, straps, or other tools to ensure close contact between the tactile device/motor and the skin, which significantly reduces the comfort and convenience of the interaction¹⁶⁹. To address this issue, some research teams have improved existing rigid motors by embedding key components (e.g. coils and permanent magnets) into elastic materials and using elastomeric materials as support structures to create flexible vibrotactile devices¹⁷⁶⁻¹⁷⁸. Thanks to the intrinsic properties of the elastic material, the aforementioned tactile devices exhibit good flexibility and stretchability, enabling them to adapt to the curvature of different skin surfaces. Moreover, the elastic modulus of the silicone material is close to that of the human skin, which allows the vibrotactile device to fit closely to the skin surface and provide stable and reliable vibrotactile feedback to the user.

In addition to electromagnetic-based actuators, pneumatic actuators can also provide mechanical vibration stimulation^{179–181}. The frequency and amplitude of mechanical vibrations can be regulated by controlling the opening and closing period of the pneumatic valve and the amount of air pressure¹⁸². Compared to electromagnetic-based actuators, pneumatic actuators have a lower driving frequency (generally below 260Hz¹⁸¹), but can cover most of the perceptual range of the mechanoreceptors and basically meet the needs of vibrotactile interaction. At the same time, pneumatic actuators have the advantage of being simple, easy to prepare, soft, and wearable, which allows them to be easily attached to the skin surface to provide stable mechanical stimulation. However, pneumatic actuators require bulky auxiliary devices such as air pumps and valves, making it difficult to meet the demand for miniaturization and lightweight of the



Fig. 12 | Tactile sensors with different transduction mechanisms. a Resistive Sensor. Reproduced with permission²⁰⁴. Copyright 2014, American Chemical Society. **b** Capacitive Sensor. Reproduced with permission¹⁹⁶. Copyright 2014, Springer Nature. **c** Piezoelectric Sensor. Reproduced with permission²²⁵. Copyright 2018, IOP Publishing. **d** Electromagnetic Sensor. Reproduced with permission²³⁷.

Copyright 2021, AAAS. e Temperature Sensor. Reproduced with permission²⁵¹. Copyright 2015, Springer Nature. f Optoelectronic Sensor. Reproduced with permission²⁵³. Copyright 2019, AAAS. g Triboelectric Sensor. Reproduced with permission²⁵⁷. Copyright 2012, American Chemical Society.

AE-Skin. In addition, some researchers have experimented with other types of actuators to present mechanical vibration stimuli. Among them, EAP actuators have received a lot of attention because of their combination of flexibility, large displacement, miniaturization, high response frequency, and low power consumption^{183–185}. Some researchers have developed vibrotactile devices based on EAP actuators that provide rich feedback to the user by controlling the frequency and amplitude of the excitation voltage^{186,187}. However, EAP actuators have problems such as high drive voltage, poor safety, and limited wearability, making them difficult to apply on a large scale.

Tactile sensors for AE-Skin

Transduction mechanisms of tactile sensors. Since the 1970s, researchers have been exploring sensors with tactile sensing capabilities and attempting to apply them in potential human-computer interaction scenarios such as prosthetics¹⁸⁸ and computer screens¹⁸⁹, laying a solid foundation for the further development and application of tactile sensors. However, most of these sensors were composed of rigid materials with low spatial resolution, limited to performing preliminary interactive operations. With the continuous progress of materials and fabrication processes, flexible and stretchable electronic devices have made significant breakthroughs and advancements in the following two decades, propelling the rapid development of flexible tactile sensing and its wide applications in fields such as robotics^{190,191}, healthcare^{192,193}, and humancomputer interaction^{194,195}. Since the 21st century, various research institutions have successively developed large-area, low-cost, and highperformance flexible tactile sensors based on different conduction mechanisms. According to different conduction mechanisms, existing flexible tactile sensors can be mainly categorized into four types: resistivebased, capacitive-based, piezoelectric-based, and electromagnetic-based tactile sensors. This classification is helpful for researchers comprehending the fundamental working principles of tactile sensors. The details of some representative tactile sensors are presented in Fig. 12 and Table 4.

Piezoresistive sensors: Piezoresistive sensors measure interactive information based on the resistive effect. Under external stress, the

resistance of the resistive material changes, and the applied force can be measured based on the resistance variation. Piezoresistive sensors have been extensively researched due to their advantages of simple structure, low power consumption, and wide detection range¹⁹⁶⁻¹⁹⁸. However, they suffer from non-linear response, fatigue, and significant sensing hysteresis. Existing studies have shown that materials such as silicon, carbon nanotubes, carbon black, and graphene¹⁹⁹⁻²⁰³ undergo changes in their energy band structures and carrier mobility under external stress, leading to changes in resistance. In addition to the energy band structure, the shape change of the sensing material can also alter the sensor's resistance²⁰⁴⁻²⁰⁶. For example, piezoresistive sensors composed of silicone rubber tubes and liquid alloys can monitor various deformations such as compression, bending, stretching, and torsion by changing the cross-sectional area of the silicone rubber tubes, exhibiting features of flexibility, stretchability, high sensitivity, high stability, and ultra-high resolution (5 mN)²⁰⁶. Furthermore, the resistance variation is also related to the contact area between components, enabling the detection of weak pressures²⁰⁷⁻²⁰⁹. Bao et al.¹⁹⁶ developed a high-precision tactile sensor based on an elastic microstructure thin film with hollow spheres. This sensor can achieve ultra-high sensitivity pressure detection by monitoring the resistance variation between the structural film and the electrodes.

Capacitive sensors: Capacitive sensors consist of two parallel electrodes and a dielectric layer sandwiched between them. Under external mechanical stimuli, the storage capacitance changes, realizing the detection of normal force²¹⁰, shear force²¹¹, and strain²¹². Capacitive sensors offer advantages such as high sensitivity, high spatial resolution, large dynamic detection range, and low power consumption^{3,213,214}. However, capacitive sensors are susceptible to noise interference and have parasitic capacitance, so they are not suitable for operation in strong electromagnetic field environments²¹⁵. In 2012, Wong et al.²¹⁶ developed a capacitive sensor based on flexible electrodes. These electrodes are made by soft lithography, and the internal microfluidic channels of the electrodes are filled with liquid alloys. Compared with rigid electrodes, flexible electrodes have the advantages of antifatigue, large curvature deformation, and anti-bending. In addition to flexible electrodes, the introduction of dielectric materials has gradually

Table 4 Summa	ry of performan	ice of repres	entativ	e tactile sensor	s reported in	the literature						
Sensing principle	Sensor size	Resolution	Array	Sensing signal	Sensing range	Sensitivity	Response time	Working life	Softness	Stretchability	Thickness	Ref.
Resistive Sensor	10 mm * 10 mm	/	3*3 3	Normal force; Shear force	0.2–59 kPa	2.21 N ⁻¹ for a normal pressure of 65 Pa	~10 ms	1	~	~	500 µm	204
	6 mm * 6 mm	6 mm	8*8	Normal force	0-5 kPa	~56.0-133.1 kPa ⁻¹	>50 ms	8000	≻	z	181 µm	196
Capacitive Sensor	5 mm * 5 mm	/	/	Normal force	>1.5 Pa	0.51kPa ⁻¹	0.15 s	10000	~	z	_	218
Piezoelectric Sensor	20 mm * 30 mm	3 mm	2*2	Axial pressure	0–2 N	0.3738 V/N (X axis), 0.4146 V/N (Y axis), 0.3443 V/N (Z axis)	/	/	~	z	3 mm	225
Electromagnetic Sensor	5 mm * 5 mm	0.1 mm	3*3	Normal force; Shear force	/	0.01 kPa ⁻¹ (Normal force) 0.1 kPa ⁻¹ –0.27 kPa ⁻¹ (Shear force)	15 ms	30000	z	z	500 µm	237
Temperature Sensor	20 mm * 30 mm	1 mm ; <0.1 K	12*12	Temperature; Nor- mal force	0-130 °C 0.1-20 kPa	28.9 kPa ⁻¹	<2 s (Tempera- ture) <20 ms (Nor- mal force)	10000	≻	z	500 µm	251
Optoelectronic Sensor	42 mm * 16.875 mm * 22 mm	0.3 N ; 0.71 mm	~	Normal force; Strain	0.5N-22N	1	/	/	≻	z	22 mm	253
Triboelectric Sensor	30 mm * 30 mm	/	_	Normal force	>13mPa-	/	100 ms	10000	7	×	460 µm	257

become an important direction for the development of capacitive sensors^{210,217}. In 2020, Sharma et al.²¹⁸ used composite nanofiber materials as the dielectric layer to create a sensitive, low-cost, and reliable ultra-low-pressure flexible capacitive sensor. This sensor achieved linear measurement within a wide pressure range of 0–400 kPa, with a sensitivity of 0.51 kPa-1 and a minimum detectable pressure of 1.5 Pa. It can be used to monitor weak physiological signals such as pulse, respiration, muscle movement, and eye movement. The dielectric materials lay the technological foundation for the research and development of next-generation high-performance human-machine interaction devices.

Piezoelectric sensors: Piezoelectric sensors utilize the piezoelectric effect of materials to measure external stimuli. Under external mechanical stress, polarization occurs within the piezoelectric material, generating opposite charges on its upper and lower surfaces. The measurement of this potential difference enables the monitoring of external stress. Piezoelectric tactile sensors offer the advantages of high sensitivity, fast response, good dynamic performance, and low power consumption. They are widely used in the measurement of dynamic signals, such as vibration and slip²¹⁹⁻²²¹. However, they face challenges related to sensitivity to temperature and humidity environments, and the inability to measure static signals. The piezoelectric constant is an important parameter for evaluating the energy conversion of piezoelectric materials. The higher the piezoelectric constant, the better the performance of the flexible tactile sensor. Inorganic materials have higher piezoelectric constants but limited flexibility, making them unsuitable for being deployed on curved surfaces. In recent years, researchers have developed piezoelectric polymer materials with high piezoelectric constants and constructed microstructures to fabricate highperformance piezoelectric sensors²²²⁻²²⁴. For instance, Chen et al.²²⁵ proposed a piezoelectric-enhanced tactile sensor based on polyvinylidene fluoride-trifluoroethylene microcolumns. Vertically aligned microcolumns are fixed between four bottom electrodes and one top electrode, and elastic protrusions are fixed on the surface of the top electrode. The microcolumn structure significantly enhances the sensitivity of the piezoelectric sensor, allowing for precise measurement of various interactive forces such as shear force, normal force, and tensile force.

Electromagnetic sensors: In contrast to other types of tactile sensors, electromagnetic sensors present various advantages, including high sensitivity, low power consumption, high reliability, robustness, and the ability to achieve three-dimensional detection²²⁶⁻²²⁸. They are widely applied in fields of robotics^{229,230}, texture discrimination²³¹⁻²³³, and healthcare^{234,235}. Electromagnetic sensors typically consist of a sensing element and an excitation magnetic field, and the detection of external stimuli is achieved by varying the intensity and direction of the excitation magnetic field²³⁶. Depending on the sensing element, magnetic sensors can be classified into various types, including Hall sensors²³⁷⁻²³⁹, anisotropic magnetoresistive (AMR) sensors^{240,241}, giant magnetoresistive (GMR) sensors²⁴²⁻²⁴⁴, and more. For example, Hall sensors are based on the Hall effect, where the carriers in a metal conductor or semiconductor produce a transverse potential difference under the influence of a magnetic field. The changes in the magnetic field can be calculated by measuring this potential difference. Hall sensors have a large magnetic field detection range and can be used for detecting strong magnetic fields. The excitation magnetic field is typically provided by rigid permanent magnets^{245,246}, flexible magnetic units^{247,248}, and electromagnetic coils^{249,250}. Compared to rigid permanent magnets, flexible magnetic units or electromagnetic coils can provide variable excitation magnetic fields by changing the proportion of magnetic particles or the magnitude of the current, thus further enlarging the measurement range of electromagnetic sensors. Additionally, flexible electromagnetic units have the advantages of miniaturization and ease of fabrication. They can be prepared in different shapes and sizes to meet various application requirements. Moreover, their inherent mechanical characteristics provide magnetic sensors with excellent flexibility.

Other transduction techniques: In addition to the aforementioned four methods, other transduction methods have been explored for the development of flexible tactile sensors. Temperature sensors based on thermoelectric materials consist of P-type and N-type semiconductors. Under the effect of a temperature gradient, thermoelectric sensors generate a thermoelectric potential on both sides, directly converting the thermal signal into an electrical signal for temperature measurement. They can be widely applied in wearable devices and the healthcare field^{251,252}. Optical sensors, on the other hand, consist of a light source, a transmission medium, and a detector. When subjected to external tactile stimuli, the intensity and wavelength of light in the transmission medium change, and the detector converts the collected light signal into an electrical signal, enabling the measurement of tactile information²⁵³⁻²⁵⁶. In the operation of these sensors, an external power source is required, which may not only increase the size and mass of the sensor but also reduce its flexibility and stretchability. A promising solution is selfpowered tactile sensors, which are based on the principles of triboelectricity or electrostatic induction²⁵⁷⁻²⁵⁹. Since these sensors can scene interactive information without the external power source, self-powered tactile sensors that utilize triboelectrification or electrostatic induction have great potential to improve the integration and application feasibility of tactile devices.

Typical interaction signal of tactile sensors. During the interaction between humans and the external environment, various tactile information can be perceived through the skin, enabling the effortless accomplishment of complex tasks. To meet the diverse interaction requirements between users and the physical/digital worlds, AE-Skin needs to possess sensing capabilities akin to human skin, capable of detecting and recognizing multiple physical stimuli, including contact pressure, contact location, sliding velocity, tensile strain, contact temperature, etc. Based on the interaction signals, the tactile sensors can also be divided into pressure sensors, strain sensors, temperature sensors, and other types. This classification is beneficial for engineers to select the appropriate tactile sensor for their specific application scenarios.

Flexible Pressure Sensors: Compared to sensors based on other transduction mechanisms, piezoresistive and capacitive sensors not only enable the measurement of dynamic forces but also facilitate the measurement of static forces, and possess the advantages of simple structure and low fabrication cost²⁶⁰. An ideal pressure sensor should exhibit both high sensitivity and a large measurement range while maintaining the same sensitivity under different pressures. However, for highly sensitive sensors, their measurement range is usually limited, making it challenging to measure higher pressures. One feasible solution is to introduce microstructures (e.g. hemispheres, pyramids, and interlocking mechanisms²⁶¹⁻²⁶³) on the surface of the sensing layer. These microstructures can effectively enhance the sensitivity of the sensor while fulfilling a wide measurement range and high linearity^{264,265}. Additionally, due to the viscoelastic properties of the flexible sensing material, its deformation and recovery rates are different during the loading and unloading processes, resulting in measurement discrepancies (hysteresis) of the sensor under the same external load. Microstructures and porous sensing materials can effectively reduce the viscoelasticity of the material, thereby improving the sensitivity and reducing the hysteresis of the pressure sensor^{210,26}

Flexible Strain Sensors: Similar to pressure sensors, strain sensors are typically fabricated based on resistive and capacitive sensing principles. Strain sensors are usually attached to the surface of the object. When the surface of the object is stretched or bent, the strain sensors will produce corresponding deformation. Traditional resistive strain sensors are composed of metal or semiconductor materials, and they are only suitable for small strain conditions (<1%) due to their mechanical properties²⁶⁷. To measure larger tensile and bending deformations, strain sensors need to possess flexible and stretchable characteristics, with their own deformation exceeding that of the object being measured. To achieve significant deformation, an effective solution is to embed conductive materials (e.g. graphene, carbon nanotubes, and silver nanowires^{268–270}) into elastic materials to enhance the stretchability of resistive strain sensors. However, due to the viscoelastic properties of the materials, there are significant issues of

hysteresis and overshoot. Another effective solution is to inject conductive fluids (e.g. liquid alloys and ionic liquids^{271,272}) into silicone tubing or microchannels, utilizing the fluidic nature and high deformability of the conductive fluid. This allows the strain sensor to maintain excellent conductivity, low hysteresis, high durability, and high sensitivity under large strains.

Flexible Temperature Sensors: Existing temperature sensors can be categorized into three types based on the sensitive materials: resistive material-based temperature sensor, composite material-based temperature sensor, and thermoelectric material-based temperature sensor²⁷³. Among them, temperature sensors based on resistive materials are typically made of pure metals (e.g. platinum, gold, silver, and copper). The resistance of the metal material varies at different temperatures, and the external temperature can be determined by measuring the resistance variation. However, the inherent rigidity of metal materials makes it difficult to meet the requirements for flexibility and stretchability²⁶⁰. To address this challenge, researchers have adopted stretchable structures (e.g. buckling and rigid islands) to enhance the stretchability of thermal resistive sensors^{274,275}. Similar to resistive material-based temperature sensors, composite materialbased temperature sensors also operate on the principle of thermal resistance. Such sensors are made of a composite material consisting of a polymer matrix and conductive fillers. Under external excitation, the substrate material undergoes expansion and separation, resulting in an increased distance between the conductive fillers and a change in the resistance variation of the sensor^{276,277}. Temperature sensors based on thermal expansion materials exhibit significant hysteresis and are not suitable for applications with high response requirements. In contrast, thermoelectric materials generate an electric current in the circuit connection between p-type and n-type semiconductors under different temperature conditions, directly converting thermal energy into electrical energy for temperature measurement^{275,278}. Compared to the other two types of temperature sensors, thermoelectric temperature sensors do not require an external power supply, facilitating miniaturization and lightweight design.

Other Types of Sensors: In addition to sensing the pressure and tension in the normal direction, it is also crucial to measure forces in other directions. For example, in object grasping control and friction force detection, it is essential to accurately perceive shear forces to ensure accurate and safe interaction^{279,280}. To sense both the magnitude and direction of contact forces, a viable solution is to combine multiple sensing units. Under the influence of forces in different directions, both the individual sensing units and the gaps between multiple sensing units undergo deformation, and multidimensional force sensing can be achieved by measuring electrical signals from multiple sensing units simultaneously²⁸¹⁻²⁸³. Different from the above multiple sensing units, Yan et al.²³⁷ designed a self-decoupled flexible tactile sensor based on a magnetic thin film with a sinusoidal magnetization direction. This sensor utilizes a single sensing unit to measure both normal and shear forces. Moreover, based on deep learning algorithms, this sensor can achieve super-high-resolution measurement of interactive information, and its sensing resolution is 60 times higher than that of the sensing unit's resolution. Fine-textured surfaces exhibit spatial resolution and vertical height differences at the micrometer level, which makes it difficult for traditional sensors to accurately sense these topography features. Inspired by animal cilia, some researchers have developed cilia-inspired tactile sensors^{284,285}. By configuring parameters such as the height and diameter of the cilia, the cilia-inspired tactile sensor can achieve ultra-high measurement accuracy. For example, it can distinguish different roughnesses of sandpaper ranging from 9.2 um to 213 um, with a minimum detectable vertical height difference of 7 um²³². It can detect tiny contact forces as low as 1 mN, with a minimum sensing accuracy of 31 uN²⁴⁷.

Materials and fabrication methods for AE-Skin

In order to improve the performance of tactile devices, researchers have expanded the direction of exploration from conventional rigid materials to realize intelligent functional materials. This extension effectively addresses the limitations of conventional rigid materials, and increases the functionalities required for tactile devices such as richness, interactivity and invisibility that are not possible with conventional rigid materials.

Polymers are extensively utilized due to their numerous advantages, including softness, stretchability, non-toxicity, high stability, affordability, and ease of preparation. These properties have captured the interest of researchers and made polymers a preferred choice for flexible tactile device fabrication. By incorporating fillers, cross-linkers, and additives, the material properties of polymers can be tailored to meet specific requirements. Smart materials can respond to external stimuli, such as voltage, magnetic field, temperature, light, etc., and these materials have been widely used in the preparation of actuators and sensors for tactile devices. For example, electronic polymer provides functionalities through conversion between electrical and mechanical energy. Under an electric field, the large strain produced by the electronic polymer actuators can be used to provide texture patterns and vibration feedback for users. At the same time, electronic polymer can be used to prepare sensors for sensing user interaction information.

Similarly, magnetically responsive materials can convert between magnetic and electric fields according to Faraday's laws of electromagnetic induction. According to this property, magnetic actuators and magnetic sensors can be prepared to provide tactile feedback (e.g. texture display and vibration) and sense interactive information. Another smart material category includes phase change materials, such as thermal responsive materials (e.g. SMA, SMP, and artificial muscles) and optical responsive materials. When the actuators are heated or exposed to light, the phase transitions of these materials occur, resulting in a large amount of elongation or contraction. Based on this deformation characteristic, researchers have developed different texture display devices to formulate patterns. Nanomaterials have good mechanical properties, electrical properties, and low cost advantages, and are widely used in flexible and stretchable tactile sensors. The common nanomaterials used for flexible tactile sensors include nanowire-based materials, CNT-based materials, graphene-based materials, conductive polymers, etc. Based on Joule's law, nanomaterials can be also used to prepare soft thermo-resistive heaters for temperature-rendering devices. In addition, we also recommend several recent reviews that cover materials for tactile actuators and tactile sensors in greater detail^{3,286-288}.

Besides the selection of the abovementioned functional materials, the proper fabrication methods are also important in preparing the tactile actuators and sensors for AE-Skin^{286,288}. In the preparation of tactile actuators and tactile sensors, soft lithography and molding processes are widely used for creating large-area patterns with microscale resolution on flexible substrates. One advantage of these techniques is their versatility in creating patterns with different geometries and dimensions. They can be used to fabricate microscale features, such as lines, dots, or holes, as well as more complex structures, including channels, pillars, and patterns with varying heights or depths. This flexibility makes them suitable for a wide range of applications, including soft tactile displays, tactile sensors, and electronic circuits. Another advantage is the ability to create large-area patterns with high resolution. These techniques can be used to fabricate patterns over areas ranging from a few micrometers to several centimeters, depending on the size of the master mold or stamp. This enables the production of devices and systems that require both microscale resolution and large surface coverage. In addition, soft lithography and molding techniques offer advantages in terms of cost, simplicity, and scalability. The materials and equipment required for these techniques are relatively inexpensive and readily available. The process itself is relatively simple and can be performed in a standard laboratory environment without the need for specialized facilities.

In recent years, 3D printing technology has experienced significant advancements and has been widely applied in soft tactile devices. This technology, also known as additive manufacturing, allows for the creation of three-dimensional objects by layering materials based on digital designs. The application of 3D printing has revolutionized the way these devices are designed and manufactured. Traditional manufacturing methods often face challenges in producing complex geometries and intricate structures,

Research gaps and future topics

With the continuous development and progress of functional materials, sensing and actuating technologies, and fabrication processes, various skinlike prototypes for displaying textures, vibrations, and temperature, as well as skins for sensing pressure, strain, and temperature, have been developed. Although these advancements are exciting, several important challenges need to be overcome on the path to realizing the goal of ambient haptic interaction using AE-Skin.

Perception mechanisms of human skin

To develop multifunctional and high-performance AE-Skin, it is necessary to deepen our understanding on the physiological and perceptual mechanisms of human skin, including skin biomechanical models, perception thresholds, and haptic illusions. These studies are expected to establish a solid theoretical foundation for the design and performance evaluation of AE-Skin.

The process of bare-finger interaction involves contact, friction, and force transmission between the fingers and objects. Due to individual differences and different object characteristics, the biomechanical model of bare-finger interaction needs to consider geometric parameters (e.g. surface curvature and contact area), surface characteristics (e.g. roughness and friction coefficient), mechanical properties (e.g. anisotropy, Young's modulus, and Poisson's ratio), and the contact state (e.g. static contact or sliding contact). The mechanical model will be helpful in simulating the contact conditions during finger-object interactions and accurately predicting the real skin response. It might provide an important reference for the selection of actuation principles, the design of mechanical structures and performance evaluation. In addition, this mechanical model might provide guidelines for optimizing and characterizing the relationship between various parameters of the AE-Skin, such as the spatial resolution of tactile devices, holding force, deformation height, thickness, stretchability, power consumption, etc. Furthermore, in-depth research is needed to reveal the perceptual mechanisms of mechanoreceptors and the biochemical mechanisms of neural signal transmission. Although existing research has explored the functions and signal transduction of individual mechanoreceptors, it remains unclear how different types of mechanoreceptors work together and encode multiple mechanical stimuli at different levels to express complex mechanical behaviors. Additionally, how the brain decodes this multi-level information for accurate perception is another area of investigation. These studies will provide insights into the design of multimodal tactile sensors and signal processing algorithms.

Regarding perceptual mechanisms, the perceptual thresholds of singlemodal tactile perception (absolute threshold and relative threshold) have been widely studied. However, it is still unclear how the perceptual thresholds change when multiple tactile stimuli simultaneously act on the human body. Some researchers have explored the coupling effect between temperature and vibration^{289,290}, or between temperature and texture²⁹¹, providing guidance for the development of temperature-vibration and temperature-texture feedback devices. However, the coupling effects of other modalities combined with texture, vibration, and temperature are still not well understood. In addition, due to the flexibility and stretchability of AE-Skin, the effect of its softness on texture, vibration, temperature and other perception thresholds needs to be further studied. This not only relates to the design of multidimensional sensor arrays but also to the integration strategies of multiple actuators.



Fig. 13 | Development status of multimodal haptic display devices.

Haptic illusions are another aspect of perceptual mechanisms that require research. Existing studies have shown that the temperature perception of the human body is related to the presentation mode of temperature stimuli^{292,293}. When harmless heat stimuli (36–42 °C) and cold stimuli (18–24 °C) alternate on the human hand, a burning sensation is perceived by the human skin. This temperature haptic illusion is highly stable and robust, with research indicating that 70 to 90% of subjects experience this haptic illusion phenomenon. Furthermore, haptic illusions based on texture, vibration, and multimodal stimulation have also been demonstrated^{294,295}. However, it is necessary to effectively utilize these tactile illusions to develop innovative interactions. On the other aspect, it is an intriguing topic to explore how to prevent misinterpretation of tactile information caused by tactile illusions.

Spatial-temporal registration among multimodal haptic stimuli

As mentioned above, many skin-like tactile devices have been developed, providing users with a single-modal interactive experience. To further enhance interaction realism, some researchers have integrated multiple actuators to achieve a synchronized presentation of multi-modal tactile information such as texture, temperature, and vibration^{67,296-302}.

Gallo et al.⁶⁷ integrated electromagnetic and piezoelectric actuators into a flexible silicone substrate to design a flexible tactile device, which can provide temperature and texture feedback. In contrast to the integration of multiple actuators, Kurogi et al.²⁹⁷ employed a single EAP actuator to achieve both temperature and vibration feedback. Under low-frequency voltage excitation, the EAP actuator generates vibrational stimuli, while under high-frequency voltage excitation (>20 kHz), the actuator generates heat based on the dielectric heating effect. The reuse of the actuator reduced the volume and structural complexity of the tactile device. However, only a single modality can be presented at any given moment, and multiple stimuli cannot be rendered simultaneously. As shown in Fig. 13, although a few studies have achieved multimodal tactile presentation, the number and the fidelity of multimodal presentation still differ from the ideal goal of AE-Skin, requiring further research in structural design, mode registration, and power supply.

In terms of structural design, careful consideration should be given to the spatial arrangement of different actuators to ensure that they do not interfere with each other and ensure the simultaneous presentation of multimodal stimuli. For example, when Paltier and shape memory actuators are used for temperature and texture rendering, insulation measures are needed to prevent the heat generated by Paltier from affecting the performance of the shape memory actuators. In addition, the layout of different actuators also needs to meet the requirements of spatial registration, ensuring that users can perceive multiple tactile stimuli within a certain contact area (a small contact area on the fingertip). For example, when simulating the tactile experience of a marble surface, it is important to consider the spacing between the actuators that are responsible for rendering temperature and texture, ensuring that the user experiences the sensation of coldness while also perceiving the texture of the marble surface.

In addition to spatial registration, multimodal tactile stimuli also need to meet the requirements of temporal and even semantic registration to provide users with more natural and realistic tactile experiences. In the temporal dimension, different actuators have different response times, such as the slow response of Pertier and the faster response of electromagnetic actuators. The control system of AE-Skin needs to control different actuators to achieve temporal alignment of different tactile stimuli. Furthermore, different tactile stimuli represent different semantic information. Temperature represents the degree of hotness or coldness, and texture represents the roughness of an object's surface. In the interaction process, different tactile stimuli need to be reasonably matched with the interaction context to enhance the realism and naturalness of the interaction, so as to ensure that the user's interaction experience is close to the real world.

Furthermore, energy consumption needs to be considered during the design process of AE-Skin. First, in the selecting of the actuating methods, low-energy consumption actuators should be adopted while meeting the performance requirements. Second, in terms of power supply, reasonable power supply methods should be chosen based on different interaction contexts. For example, when AE-Skin is applied to wearable devices or mobile devices, ultra-thin batteries or wireless power supply technologies can be selected¹⁷⁶. When AE-Skin is attached to fixed surfaces such as touch screens in electronic cars, external power supply methods can be adopted. Thanks to high energy density, high power density, and long cycle life, Lithiumion batteries are adopted as one of the most conventional power sources, and are widely used for tactile devices^{177,178,303,304}. Despite their many advantages, the inflexible nature of Lithiumion batteries can restrict the flexibility and stretchability of tactile devices³⁰⁵. It is desirable to develop a promising power method for realizing thin and stretchable tactile devices. Near-field communication is a highly promising solution for power delivery, as it enables wireless power transfer over short distances. This eliminates the need for traditional wired power delivery methods, providing greater flexibility and portability for tactile devices¹⁷⁶. Another alternative solution is the stretchable batteries with excellent flexibility, mechanical stability and electrochemical performance. In the last decade, stretchable batteries have shown great potential for haptics and have integrated into various wearable electronics and tactile devices^{306–309}.

Integration between sensing and actuating units

To achieve the natural interaction between users and objects, AE-Skin needed to be able to simultaneously sense the user's interactive behavior and provide multimodal tactile stimuli. To achieve this goal, the sensing and actuating units need to be integrated within the confined contact area covered by a fingertip. Different from the single-mode tactile sensor or tactile rendering device, the design and fabrication of the actuating-sensing integrated AE-Skin require careful consideration of the following issues: spatial layout, spatial registration, and functional compatibility to avoid mutual interference of sensing and actuating components at the spatial and signal levels. Fig. 14 illustrates the functions and spatial resolutions of some existing tactile devices.

For actuating-sensing integrated AE-Skin, the first challenge lies in the spatial layout of the actuators and sensors to ensure that the actuating signals and sensing signals do not interfere with each other. A widely used layout is to place the sensors above the drivers^{182,310-313}, which allows the sensors to directly contact users' fingertips, facilitating reliable tactile sensing. However, the overhead sensor might obstruct the movement of the actuators, thus impairing the performance of the tactile actuators. Conversely, when the actuators are positioned above the sensors, the actuators can provide the



user with sufficient tactile stimuli³¹⁴. However, the presence of actuators may also impede the transmission of the user's interactive information. When the force or temperature is transferred from the user's fingertip to the tactile sensor, the interactive information may be attenuated, which can increase the measurement difficulty and reduce the measurement accuracy. To avoid mutual interference between the actuators and sensors, an effective solution is to alternately distribute the driver and the sensor on the same horizontal plane^{315,316}. Compared to the first two layouts, the alternating horizontal layout requires a larger area for arranging the actuators and sensors, which might reduce the spatial resolution of the tactile device, inducing a challenge for the spatial registration of the actuators and sensors. To achieve spatial registration, it is necessary to ensure that the contact area between the fingertip and the AE-Skin can cover at least one actuator and one sensor under any interaction positions. In this case, when the fingertip interacts with the AE-Skin, the user can not only perceive the tactile stimuli from the actuators but also trigger the sensing signals of the sensors. Therefore, the size of the actuators and sensor needs to be small enough to improve the spatial resolution of the tactile device to meet the requirements of spatial registration.

In addition to spatial registration, it is also necessary to consider the compatibility of different components' performance to avoid mutual interference when they work simultaneously. For example, when the electromagnetic actuator is used for texture display, the use of magnetic sensors, piezoelectric sensors, and capacitive sensors should be avoided to ensure that the electromagnetic field generated by the electromagnetic actuators does not interfere with the sensing signal, thereby affecting the accuracy and sensitivity of the tactile sensors. Furthermore, to achieve a large-sized and high-spatial-resolution AE-Skin, efficient and real-time control of high-density large-scale arrays of actuators and sensors, ranging from thousands to millions or even more, needs to be addressed. To meet the large-scale control requirements, it is necessary to study the flexible and even stretchable circuit, signal line routing design, and high-performance control board.

Spatial-temporal registration between visual and haptic display

Unlike the physical world, when AE-Skin is applied to the digital world such as providing dynamic tactile feedback on a touch screen, it needs to be matched with the digital environment to provide consistent visual-tactile experiences to users, which imposes more requirements on the performance of AE-Skin. Therefore, it is necessary to consider the transparency, thickness, stretchability and virtual-real registration to ensure that the AE-Skin does not affect the visual information and touch-sensing functionality of the screens. Fig. 15 depicts the current state of existing tactile devices with respect to transparency, stretchability, and thickness.

When AE-Skin is attached to screens such as smartphones, iPads, incar displays, and large-sized LED screens, it needs to have high transparency to ensure that it does not obstruct or affect the visual information presented on the screens, thus avoiding any negative impact on the user's interaction experience. Therefore, it is necessary to select high transparency of the substrate material, actuators and sensors in the design of AE-Skin. For example, transparent and stretchable polydimethylsiloxane (PDMS) can be chosen as the substrate material, pneumatic actuators can provide tactile feedback to users, and transparent sensors based on materials such as silver nanowires¹²⁷, graphene³¹⁷, and carbon nanotubes³¹⁸ can be used to capture user's interaction behavior. Additionally, the AE-Skin should be as thin as possible to avoid compromising the touch-sensing functionality of the screen. Otherwise, thicker AE-Skin may prevent the formation of coupling capacitance between the finger and the touch screen, making it difficult to generate induced currents for detecting the finger's contact position.

In virtual interactive scenes, visual-tactile fusion is one of the key technologies for achieving immersive experiences. Due to significant differences between virtual environments and real environments, there are still some challenges to be addressed in visual-tactile fusion. Firstly, there is a certain time delay in the generation and transmission of virtual visual and tactile signals, which may result in a mismatch between the perceived visual and tactile information in the temporal dimension, causing discomfort or even adverse reactions such as dizziness and nausea. Secondly, both the user's and the virtual avatar's positions are constantly changing during the interaction process. The sensors of the AE-Skin need to dynamically and accurately measure the user's pose changes to ensure the precise matching of visual and tactile information regarding the positions and orientations of the virtual avatar and the real finger, ensuring the interaction experience consistency of the virtual and real space. Additionally, AE-Skin also needs to possess flexibility and stretchability to ensure its suitability for simulating objects with different shapes and curvatures, ensuring a good fit with the surface of the object without affecting its shape, size, and other attributes. For example, one important application scenario is to attach the AE-Skin on the surface of a shape display device to formulate "digital clay"¹⁹, which can provide multi-modal tactile stimuli for supporting bare-hand interaction with virtual objects.

Considering the technological maturity, potential application value, and societal impact, these future topics have been further refined into shortterm and long-term goals. In the short term, significant advancements are required in the following aspects. First, user studies should be conducted to



Fig. 15 | Current state of existing tactile devices with respect to transparency, stretchability, and thickness. The height of the colored bar refers to the relative thickness of each tactile device, and the value within/or under the colored bar represents the absolute thickness of the device.

explore the effect of the multi-modal tactile stimuli on the perceptual thresholds and haptic illusion. Second, the minimization and performance improvement should be carried out by fully exploiting the potential of the existing actuators and sensors. Third, it is essential to take into account the spatial arrangement of various actuators, as well as the layout among actuators and sensors, to avoid mutual interference. Fourth, the temporal and semantic registration of multi-modal tactile stimuli should be considered to ensure that the representation of different tactile stimuli is consistent with the actual interaction scenarios. Based on these short-term studies, it is possible to develop a preliminary version of AE-Skin to provide users with a more immersive, realistic interactive experience.

In the long term, more time and effort need to be invested to make a breakthrough in the following aspects. In the perception mechanism, a biomechanics model needs to be constructed to simulate and analyze the force transmission and skin deformation when the finger is in contact with the object. Further, a comprehensive investigation is required to reveal the underlying perceptual mechanisms of mechanoreceptors and the biochemical mechanisms of neural signal transmission. In terms of advanced materials, it is necessary to explore other functional materials with high transparency, ultra-thin, and large stretchability. In addition, the development of ultra-thin, flexible, and high-capacity energy storage materials is a significant advancement toward addressing the challenge of energy consumption. In VR applications, it is crucial to conduct in-depth studies on visual-tactile registration to minimize mismatch between the visual and tactile information and prevent adverse reactions during prolonged usage. The solutions to these long-term challenges will propel the development of human-computer interaction, ushering human beings into an ambient haptic world.

Data availability

All the data are available within the article or available from the authors upon reasonable request.

Received: 14 January 2024; Accepted: 29 March 2024; Published online: 02 May 2024

References

- Weiser, M. The computer for the 21st century. ACM SIGMOBILE Mob. Comput. Commun. Rev. 3, 3–11 (1999).
- MacLean, K. E. Putting haptics into the ambience. *IEEE Trans. Haptics* 2, 123–135 (2009).
- Hammock, M. L. et al. 25th anniversary article: the evolution of electronic skin (e-skin): a brief history, design considerations, and recent progress. *Adv. Mater.* 25, 5997–6038 (2013).
- 4. Wang, X. et al. Recent progress in electronic skin. *Adv. Sci.* **2**, 1500169 (2015).
- Chang, K.-J. et al. Development of haptic vibration system for steering wheel using soft actuators. *Trans. Korean Soc. Automot. Eng.* 31, 607–612 (2023).
- Kim, H., Nam, J., Kim, M. & Kyung, K.-U. Wide-bandwidth soft vibrotactile interface using electrohydraulic actuator for haptic steering wheel application. *IEEE Robot. Autom. Lett.* 6, 8245–8252 (2021).
- Kern, D. et al. Enhancing Navigation Information with Tactile Output Embedded into the Steering Wheel. in *Pervasive Computing* (eds. Tokuda, H. et al.) 5538 42–58 (Springer Berlin Heidelberg, 2009).
- Luo, Y. et al. Intelligent Carpet: Inferring 3D Human Pose from Tactile Signals. In 2021 IEEE/CVF Conference on Computer Vision and Pattern Recognition (CVPR) 11250–11260 (IEEE, 2021).
- Chaccour, K., Darazi, R., Hajjam El Hassans, A. & Andres, E. Smart carpet using differential piezoresistive pressure sensors for elderly fall detection. In 2015 IEEE 11th International Conference on Wireless and Mobile Computing, Networking and Communications (WiMob) 225–229 (IEEE, 2015).
- Ayyildiz, M. et al. Contact mechanics between the human finger and a touchscreen under electroadhesion. *Proc. Natl Acad. Sci.* 115, 12668–12673 (2018).
- Ghenna, S. et al. Enhancing variable friction tactile display using an ultrasonic travelling wave. *IEEE Trans. Haptics* 10, 296–301 (2017).

- 12. Nai, W. et al. Vibrotactile feedback rendering of patterned textures using a waveform segment table method. *IEEE Trans. Haptics* **14**, 849–861 (2021).
- Qi, J. et al. HaptGlove—untethered Pneumatic glove for multimode haptic feedback in reality–virtuality continuum. *Adv. Sci.* 10, 2301044 (2023).
- Hinchet, R., Vechev, V., Shea, H. & Hilliges, O. DextrES: Wearable haptic feedback for grasping in VR via a thin form-factor electrostatic brake. in *Proc. 31st Annual ACM Symposium on User Interface Software and Technology* 901–912 (ACM, 2018).
- 15. Baik, S., Park, S. & Park, J. Haptic gove using tendon-driven soft robotic mechanism. *Front. Bioeng. Biotechnol.* **8**, 541105 (2020).
- Gonzalez, E. J., Ofek, E., Gonzalez-Franco, M. & Sinclair, M. X-Rings: A hand-mounted 360° shape display for grasping in virtual reality. In *The 34th Annual ACM Symposium on User Interface Software and Technology* 732–742 (ACM, 2021).
- Sun, Y., Yoshida, S., Narumi, T. & Hirose, M. PaCaPa: A Handheld VR device for rendering size, shape, and stiffness of virtual objects in tool-based interactions. In *Proc. 2019 CHI Conference on Human Factors in Computing Systems* 1–12 (ACM, 2019).
- Whitmire, E. et al. Haptic revolver: touch, shear, texture, and shape rendering on a reconfigurable virtual reality controller. In *Proc. 2018 CHI Conference on Human Factors in Computing Systems* 1–12 (ACM, 2018).
- 19. Wang, D., Ohnishi, K. & Xu, W. Multimodal haptic display for virtual reality: a survey. *IEEE Trans. Ind. Electron.* **67**, 610–623 (2020).
- Hollins, M. & Risner, S. R. Evidence for the duplex theory of tactile texture perception. *Percept. Psychophys.* 62, 695–705 (2000).
- Weber, A. I. et al. Spatial and temporal codes mediate the tactile perception of natural textures. *Proc. Natl Acad. Sci.* **110**, 17107–17112 (2013).
- Basdogan, C., Giraud, F., Levesque, V. & Choi, S. A review of surface haptics: enabling tactile effects on touch surfaces. *IEEE Trans. Haptics* 13, 450–470 (2020).
- 23. Bar-Cohen, Y. Electroactive polymers as an enabling materials technology. *Proc. Inst. Mech. Eng. Part G J. Aerosp. Eng.* **221**, 553–564 (2007).
- 24. Pelrine, R., Kornbluh, R., Pei, Q. & Joseph, J. High-speed electrically actuated elastomers with strain greater than 100%. *Science* **287**, 836–839 (2000).
- Yun, G.-Y., Kim, J., Kim, J.-H. & Kim, S.-Y. Fabrication and testing of cellulose EAPap actuators for haptic application. *Sens. Actuators Phys.* **164**, 68–73 (2010).
- Kovacs, G., Düring, L., Michel, S. & Terrasi, G. Stacked dielectric elastomer actuator for tensile force transmission. *Sens. Actuators Phys.* **155**, 299–307 (2009).
- Pelrine, R. E., Kornbluh, R. D. & Joseph, J. P. Electrostriction of polymer dielectrics with compliant electrodes as a means of actuation. *Sens. Actuators Phys.* 64, 77–85 (1998).
- 28. Bai, H., Li, S. & Shepherd, R. F. Elastomeric haptic devices for virtual and augmented reality. *Adv. Funct. Mater.* **31**, 2009364 (2021).
- 29. Phung, H. et al. Tactile display with rigid coupling based on soft actuator. *Meccanica* **50**, 2825–2837 (2015).
- Leroy, E., Hinchet, R. & Shea, H. Multimode hydraulically amplified electrostatic actuators for wearable haptics. *Adv. Mater.* 32, 2002564 (2020).
- 31. Frediani, G., Busfield, J. & Carpi, F. Enabling portable multiple-line refreshable Braille displays with electroactive elastomers. *Med. Eng. Phys.* **60**, 86–93 (2018).
- Ankit et al. Highly transparent and integrable surface texture change device for localized tactile feedback. *Small* 14, 1702312 (2018).
- Koo, I. et al. Wearable tactile display based on soft actuator. In Proc. 2006 IEEE International Conference on Robotics and Automation, 2006. ICRA 2006. 2220–2225 (IEEE, 2006).

- Mun, S. et al. Electro-active polymer based soft tactile interface for wearable devices. *IEEE Trans. Haptics* 11, 15–21 (2018).
- Lee, H. S. et al. Design analysis and fabrication of arrayed tactile display based on dielectric elastomer actuator. *Sens. Actuators Phys.* 205, 191–198 (2014).
- Ji, X. et al. An autonomous untethered fast soft robotic insect driven by low-voltage dielectric elastomer actuators. *Sci. Robot.* 4, eaaz6451 (2019).
- Sheima, Y., Caspari, P. & Opris, D. M. Artificial muscles: dielectric elastomers responsive to low voltages. *Macromol. Rapid Commun.* 40, 1900205 (2019).
- 38. Poulin, A., Rosset, S. & Shea, H. R. Printing low-voltage dielectric elastomer actuators. *Appl. Phys. Lett.* **107**, 244104 (2015).
- Han, A. K., Ji, S., Wang, D. & Cutkosky, M. R. Haptic surface display based on miniature dielectric fluid transducers. *IEEE Robot. Autom. Lett.* 5, 4021–4027 (2020).
- Acome, E. et al. Hydraulically amplified self-healing electrostatic actuators with muscle-like performance. Science 359, 61–65 (2018).
- 41. Kim, Y. et al. Printing ferromagnetic domains for untethered fasttransforming soft materials. *Nature* **558**, 274–279 (2018).
- 42. Xu, T. et al. Millimeter-scale flexible robots with programmable three-dimensional magnetization and motions. *Sci. Robot.* **4**, eaav4494 (2019).
- 43. Lu, H. et al. Battery-less soft millirobot that can move, sense, and communicate remotely by coupling the magnetic and piezoelectric effects. *Adv. Sci.* **7**, 2000069 (2020).
- Shinohara, M., Shimizu, Y. & Mochizuki, A. Three-dimensional tactile display for the blind. *IEEE Trans. Rehabil. Eng.* 6, 249–256 (1998).
- Sojib, N. & Zafar Iqbal, M. Single cell bangla braille book reader for visually impaired people. In 2018 International Conference on Bangla Speech and Language Processing (ICBSLP) 1–4 (IEEE, 2018).
- Bolzmacher, C. et al. Tactile refreshable screen based on magnetorheological fluids for map exploration and navigation tasks. In *Proceedings Volume 8066, Smart Sensors, Actuators, and MEMS V* (eds. Schmid, U., Sánchez-Rojas, J. L. & Leester-Schaedel, M.) 80661T (2011).
- 47. Fukuda, T. et al. Micro resonator using electromagnetic actuator for tactile display. In 1997 International Symposium on Micromechanics and Human Science (Cat. No.97TH8311) 143–148 (IEEE, 1997).
- Streque, J. et al. Elaboration and test of high energy density magnetic micro-actuators for tactile display applications. *Procedia Chem.* 1, 694–697 (2009).
- Bettelani, G. C. et al. Design and validation of the *readable* device: a single-cell electromagnetic refreshable braille display. *IEEE Trans. Haptics* 13, 239–245 (2020).
- 50. Strasnick, E. & Follmer, S. Applications of switchable permanent magnetic actuators in shape change and tactile display. in *Proceedings of the 29th Annual Symposium on User Interface Software and Technology* 123–125 (ACM, 2016).
- Benali-Khoudja, M., Hafez, M. & Kheddar, A. Vital: an electromagnetic integrated tactile display. *Displays* 28, 133–144 (2007).
- 52. Zarate, J. J. & Shea, H. Using pot-magnets to enable stable and scalable electromagnetic tactile displays. *IEEE Trans. Haptics* **10**, 106–112 (2017).
- Streque, J., Talbi, A., Pernod, P. & Preobrazhensky, V. Pulse-driven magnetostatic micro-actuator array based on ultrasoft elastomeric membranes for active surface applications. *J. Micromech. Microeng.* 22, 095020 (2012).
- 54. Streque, J., Talbi, A., Pernod, P. & Preobrazhensky, V. New magnetic microactuator design based on pdms elastomer and mems technologies for tactile display. *IEEE Trans. Haptics* **3**, 88–97 (2010).
- Guo, Y. et al. Mrs-tex: a magnetically responsive soft tactile device for texture display. *IEEE Trans. Ind. Electron.* 69, 11531–11540 (2022).

- Guo, Y. et al. Electromagnetic-actuated soft tactile device using a pull–push latch structure. *IEEE Trans. Ind. Electron.* **70**, 10344–10352 (2023).
- Xiao F., Zhao K., & Sun L. *Electromagnetic Compatibility in Integrative Motor System* (eds. Xiao F. et al.) 33–35 (National Defence Industry Press, 2017).
- Wu Q., Fu J. & Meng F. *Principles and Techniques of Electromagnetic Compatibility* (eds. Wu Q. et al.) 75–77 (Harbin Institute of Technology Press, 2012).
- 59. Yang, W. et al. A survey on tactile displays for visually impaired people. *IEEE Trans. Haptics* **14**, 712–721 (2021).
- Vidal-Verdu, F. & Hafez, M. Graphical tactile displays for visuallyimpaired people. *IEEE Trans. Neural Syst. Rehabil. Eng.* 15, 119–130 (2007).
- Kim, J. et al. Braille display for portable device using flip-latch structured electromagnetic actuator. *IEEE Trans. Haptics* 13, 59–65 (2020).
- Kim, J., Han, B.-K. & Kwon, D.-S. 2d braille display module using rotating latch structured voice coil actuator. In *Haptic Interaction* (eds. Kajimoto, H. et al.) 223–225 (Springer Singapore, 2019).
- 63. Leonardis, D., Loconsole, C. & Frisoli, A. A passive and scalable magnetic mechanism for braille cursor, an innovative refreshable braille display. *Meccanica* **55**, 1639–1653 (2020).
- 64. Loconsole, C., Leonardis, D., Gabardi, M. & Frisoli, A. BrailleCursor: an innovative refreshable braille display based on a single sliding actuator and simple passive pins. In *2019 IEEE World Haptics Conference (WHC)* 139–144 (IEEE, 2019).
- 65. Pece, F. et al. Magtics: flexible and thin form factor magnetic actuators for dynamic and wearable haptic feedback. In *Proc. 30th Annual ACM Symposium on User Interface Software and Technology* 143–154 (ACM, 2017).
- 66. Vechev, V. et al. Tactiles: dual-mode low-power electromagnetic actuators for rendering continuous contact and spatial haptic patterns in VR. In *2019 IEEE Conference on Virtual Reality and 3D User Interfaces (VR)* 312–320 (IEEE, 2019).
- Gallo, S. et al. A flexible multimodal tactile display for delivering shape and material information. *Sens. Actuators Phys.* 236, 180–189 (2015).
- 68. Son, C. et al. A flexible multimodal tactile display array for virtual shape and texture. *Microsyst. Technol.* **22**, 2587–2594 (2016).
- Do, T. N., Phan, H., Nguyen, T. & Visell, Y. Miniature soft electromagnetic actuators for robotic applications. *Adv. Funct. Mater.* 28, 1800244 (2018).
- Jin, S. W. et al. Stretchable loudspeaker using liquid metal microchannel. *Sci. Rep.* 5, 11695 (2015).
- Kohls, N. et al. Compliant electromagnetic actuator architecture for soft robotics. In 2020 IEEE International Conference on Robotics and Automation (ICRA) 9042–9049 (IEEE, 2020).
- Sapra, P. et al. Refreshable braille display using shape memory alloy with latch mechanism. In *Volume 9: 13th ASME/IEEE International Conference on Mechatronic and Embedded Systems and Applications* V009T07A040 (American Society of Mechanical Engineers, 2017).
- Chaves, D. R. et al. Microtuators of sma for braille display system. In 2009 IEEE International Workshop on Medical Measurements and Applications 64–68 (IEEE, 2009).
- 74. Sapra, P. et al. A compliant mechanism design for refreshable braille display using shape memory alloy. In *Volume 9: 2015 ASME/IEEE International Conference on Mechatronic and Embedded Systems and Applications* V009T07A054 (American Society of Mechanical Engineers, 2015).
- 75. Singhal, A. et al. Application of shape memory alloy (SMA) based actuation for refreshable display of braille. In *Volume 4: 18th Design* for Manufacturing and the Life Cycle Conference; 2013 ASME/IEEE International Conference on Mechatronic and Embedded Systems

and Applications V004T08A053 (American Society of Mechanical Engineers, 2013).

- Zhao, F., Fukuyama, K. & Sawada, H. Compact braille display using sma wire array. In RO-MAN 2009 – The 18th IEEE International Symposium on Robot and Human Interactive Communication 28–33 (IEEE, 2009).
- Velazquez, R., Pissaloux, E. E., Hafez, M. & Szewczyk, J. Tactile rendering with shape-memory-alloy pin-matrix. *IEEE Trans. Instrum. Meas.* 57, 1051–1057 (2008).
- Matsunaga, T. et al. 2-d and 3-d tactile pin display using sma microcoil actuator and magnetic latch. In *The 13th International Conference on Solid-State Sensors, Actuators and Microsystems,* 2005. Digest of Technical Papers. TRANSDUCERS '05. 1 325–328 (IEEE, 2005).
- Matsunaga, T., Totsu, K., Esashi, M. & Haga, Y. Tactile display using shape memory alloy micro-coil actuator and magnetic latch mechanism. *Displays* 34, 89–94 (2013).
- Matsunaga, T., Totsu, K., Esashi, M. & Haga, Y. Tactile display for 2-d and 3-d shape expression using sma micro actuators. In 2005 3rd IEEE/EMBS Special Topic Conference on Microtechnology in Medicine and Biology 88–91 (IEEE, 2005).
- 81. Haga, Y. et al. Dynamic braille display using sma coil actuator and magnetic latch. *Sens. Actuators Phys.* **119**, 316–322 (2005).
- Behl, M. & Lendlein, A. Shape-memory polymers. *Mater. Today* 10, 20–28 (2007).
- 83. Mather, P. T., Luo, X. & Rousseau, I. A. Shape memory polymer research. *Annu. Rev. Mater. Res.* **39**, 445–471 (2009).
- Ren, Z. et al. Phase-changing bistable electroactive polymer exhibiting sharp rigid-to-rubbery transition. *Macromolecules* 49, 134–140 (2016).
- 85. Besse, N., Rosset, S., Zarate, J. J. & Shea, H. Flexible active skin: large reconfigurable arrays of individually addressed shape memory polymer actuators. *Adv. Mater. Technol.* **2**, 1700102 (2017).
- Besse, N. et al. Understanding graphics on a scalable latching assistive haptic display using a shape memory polymer membrane. *IEEE Trans. Haptics* 11, 30–38 (2018).
- Besse, N., Zarate, J. J., Rosset, S. & Shea, H. R. Flexible haptic display with 768 independently controllable shape memory polymers taxels. In 2017 19th International Conference on Solid-State Sensors, Actuators and Microsystems (TRANSDUCERS) 323–326 (IEEE, 2017).
- Russomanno, A., Xu, Z., O'Modhrain, S. & Gillespie, B. A pneu shape display: physical buttons with programmable touch response. In 2017 IEEE World Haptics Conference (WHC) 641–646 (IEEE, 2017).
- 89. Russomanno, A., Gillespie, R. B., O'Modhrain, S. & Burns, M. The design of pressure-controlled valves for a refreshable tactile display. In 2015 IEEE World Haptics Conference (WHC) 177–182 (IEEE, 2015).
- Russomanno, A., Gillespie, R. B., O'Modhrain, S. & Barber, J. Modeling pneumatic actuators for a refreshable tactile display. In *Haptics: Neuroscience, Devices, Modeling, and Applications* (eds. Auvray, M. & Duriez, C.) 385–393 (Springer Berlin Heidelberg, 2014).
- Ujitoko, Y., Taniguchi, T., Sakurai, S. & Hirota, K. Development of finger-mounted high-density pin-array haptic display. *IEEE Access* 8, 145107–145114 (2020).
- Ota, Y. et al. Inside touch: presentation of tactile feeling inside virtual object using finger-mounted pin-array display. *IEEE Access* 9, 75150–75157 (2021).
- Wu, X. et al. A refreshable braille cell based on pneumatic microbubble actuators. *J. Microelectromechanical Syst.* 21, 908–916 (2012).
- Unger, M. A. et al. Monolithic microfabricated valves and pumps by multilayer soft lithography. *Science* 288, 113–116 (2000).
- 95. Duffy, D. C., McDonald, J. C., Schueller, O. J. A. & Whitesides, G. M. Rapid prototyping of microfluidic systems in poly(dimethylsiloxane). *Anal. Chem.* **70**, 4974–4984 (1998).

- Sia, S. K. & Whitesides, G. M. Microfluidic devices fabricated in poly(dimethylsiloxane) for biological studies. *ELECTROPHORESIS* 24, 3563–3576 (2003).
- 97. Thorsen, T., Maerkl, S. J. & Quake, S. R. Microfluidic large-scale integration. *Science* **298**, 580–584 (2002).
- Bartlett, N. W., Becker, K. P. & Wood, R. J. A fluidic demultiplexer for controlling large arrays of soft actuators. *Soft Matter* 16, 5871–5877 (2020).
- Grover, W. H., Ivester, R. H. C., Jensen, E. C. & Mathies, R. A. Development and multiplexed control of latching pneumatic valves using microfluidic logical structures. *Lab. Chip* 6, 623 (2006).
- Weaver, J. A. et al. Static control logic for microfluidic devices using pressure-gain valves. *Nat. Phys.* 6, 218–223 (2010).
- 101. Mosadegh, B. et al. Control of soft machines using actuators operated by a Braille display. *Lab Chip* **14**, 189–199 (2014).
- Heisser, R. H. et al. Valveless microliter combustion for densely packed arrays of powerful soft actuators. *Proc. Natl Acad. Sci.* 118, e2106553118 (2021).
- Camargo, C. J. et al. Batch fabrication of optical actuators using nanotube–elastomer composites towards refreshable Braille displays. *J. Micromech. Microeng.* 22, 075009 (2012).
- Torras, N. et al. Tactile device based on opto-mechanical actuation of liquid crystal elastomers. *Sens. Actuators Phys.* 208, 104–112 (2014).
- 105. Lamuta, C. et al. Digital texture voxels for stretchable morphing skin applications. *Adv. Mater. Technol.* **4**, 1900260 (2019).
- 106. Kenshalo, D. R. Correlations of temperature sensitivity in man and monkey, a first approximation. In *Sensory Functions of the Skin in Primates* 305–330 (Elsevier, 1976).
- Yarnitsky, D. & Ochoa, J. L. Warm and cold specific somatosensory systems: psychophysical thresholds, reaction times and peripheral conduction velocities. *Brain* **114**, 1819–1826 (1991).
- 108. Luo, M. et al. High-density thermal sensitivity maps of the human body. *Build. Environ.* **167**, 106435 (2020).
- Jones, L. A. & Berris, M. The psychophysics of temperature perception and thermal-interface design. In *Proc. 10th Symposium* on *Haptic Interfaces for Virtual Environment and Teleoperator Systems. HAPTICS 2002* 137–142 (IEEE Comput. Soc, 2002).
- 110. Cain, W. S. Spatial discrimination of cutaneous warmth. *Am. J. Psychol.* **86**, 169 (1973).
- 111. Hardy, J. D. & Oppel, T. W. Studies in temperature sensation. iii. the sensitivity of the body to heat and the spatial summation of the end organ responses. *J. Clin. Invest.* **16**, 533–540 (1937).
- Kenshalo, D. R., Decker, T. & Hamilton, A. Spatial summation on the forehead, forearm, and back produced by radiant and conducted heat. *J. Comp. Physiol. Psychol.* 63, 510–515 (1967).
- 113. Parida, K., Bark, H. & Lee, P. S. Emerging thermal technology enabled augmented reality. *Adv. Funct. Mater.* **31**, 2007952 (2021).
- Spray, D. C. Cutaneous temperature receptors. *Annu. Rev. Physiol.* 48, 625–638 (1986).
- 115. Rolke, R. et al. Quantitative sensory testing in the German research network on neuropathic pain (DFNS): standardized protocol and reference values. *Pain* **123**, 231–243 (2006).
- 116. Lee, J. et al. Stretchable skin-like cooling/heating device for reconstruction of artificial thermal sensation in virtual reality. *Adv. Funct. Mater.* **30**, 1909171 (2020).
- 117. Kim, D. et al. Highly stretchable and oxidation-resistive Cu nanowire heater for replication of the feeling of heat in a virtual world. *J. Mater. Chem. A* **8**, 8281–8291 (2020).
- Peiris, R. L. et al. Thermovr: exploring integrated thermal haptic feedback with head mounted displays. In *Proc. 2017 CHI Conference on Human Factors in Computing Systems* 5452–5456 (ACM, 2017).

- 119. Ho, H.-N. et al. Colour-temperature correspondences: when reactions to thermal stimuli are influenced by colour. *PLoS ONE* **9**, e91854 (2014).
- Ho, H.-N. & Jones, L. A. Contribution of thermal cues to material discrimination and localization. *Percept. Psychophys.* 68, 118–128 (2006).
- 121. Peiris, R. L., Feng, Y.-L., Chan, L. & Minamizawa, K. Thermalbracelet: exploring thermal haptic feedback around the wrist. In Proc. 2019 CHI Conference on Human Factors in Computing Systems 1–11 (ACM, 2019).
- 122. Zhu, K. et al. A sense of ice and fire: Exploring thermal feedback with multiple thermoelectric-cooling elements on a smart ring. *Int. J. Hum. -Comput. Stud.* **130**, 234–247 (2019).
- 123. Nasser, A., Zhu, K. & Wiseman, S. Thermo-haptic earable display for the hearing and visually impaired. In *The 21st International ACM SIGACCESS Conference on Computers and Accessibility* 630–632 (ACM, 2019).
- Venkatasubramanian, R., Siivola, E., Colpitts, T. & O'Quinn, B. Thinfilm thermoelectric devices with high room-temperature figures of merit. *Nature* 413, 597–602 (2001).
- 125. Hong, S. et al. Wearable thermoelectrics for personalized thermoregulation. *Sci. Adv.* **5**, eaaw0536 (2019).
- Park, H. et al. Mat-like flexible thermoelectric system based on rigid inorganic bulk materials. J. Phys. Appl. Phys. 50, 494006 (2017).
- Hong, S. et al. Highly stretchable and transparent metal nanowire heater for wearable electronics applications. *Adv. Mater.* 27, 4744–4751 (2015).
- Jang, N.-S. et al. Simple approach to high-performance stretchable heaters based on Kirigami patterning of conductive paper for wearable thermotherapy applications. ACS Appl. Mater. Interfaces 9, 19612–19621 (2017).
- 129. Zhang, X., Yan, X., Chen, J. & Zhao, J. Large-size graphene microsheets as a protective layer for transparent conductive silver nanowire film heaters. *Carbon* 69, 437–443 (2014).
- 130. Wang, Y. et al. Flexible thermoelectrics: from energy harvesting to human–machine interaction. J. Appl. Phys. **133**, 110901 (2023).
- Lee, J., Kim, D., Sul, H. & Ko, S. H. Thermo-haptic materials and devices for wearable virtual and augmented reality. *Adv. Funct. Mater.* **31**, 2007376 (2021).
- 132. DiSalvo, F. J. Thermoelectric cooling and power generation. *Science* **285**, 703–706 (1999).
- 133. Kishore, R. A. et al. Ultra-high performance wearable thermoelectric coolers with less materials. *Nat. Commun.* **10**, 1765 (2019).
- 134. Gabardi, M. et al. A high performance thermal control for simulation of different materials in a fingertip haptic device. in *Haptics: Science, Technology, and Applications* (eds. Prattichizzo, D. et al.) 313–325 (Springer International Publishing, 2018).
- 135. Lee, D. et al. Liquid-metal-electrode-based compact, flexible, and high-power thermoelectric device. *Energy* **188**, 116019 (2019).
- 136. Kim, S.-W. et al. Thermal display glove for interacting with virtual reality. *Sci. Rep.* **10**, 11403 (2020).
- 137. An, B. W. et al. Stretchable, transparent electrodes as wearable heaters using nanotrough networks of metallic glasses with superior mechanical properties and thermal stability. *Nano Lett.* **16**, 471–478 (2016).
- Cheng, Y. et al. Highly stretchable and conductive copper nanowire based fibers with hierarchical structure for wearable heaters. ACS Appl. Mater. Interfaces 8, 32925–32933 (2016).
- 139. Jung, D. et al. Transparent film heaters using multi-walled carbon nanotube sheets. *Sens. Actuators Phys.* **199**, 176–180 (2013).
- 140. Lee, Y. et al. Versatile, high-power, flexible, stretchable carbon nanotube sheet heating elements tolerant to mechanical damage and severe deformation. *Adv. Funct. Mater.* **28**, 1706007 (2018).

- Zhou, J. et al. High-ampacity conductive polymer microfibers as fast response wearable heaters and electromechanical actuators. *J. Mater. Chem. C.* 4, 1238–1249 (2016).
- 142. Choi, S. et al. Stretchable heater using ligand-exchanged silver nanowire nanocomposite for wearable articular thermotherapy. ACS Nano 9, 6626–6633 (2015).
- Liu, P. et al. Stretchable and energy-efficient heating carbon nanotube fiber by designing a hierarchically helical structure. *Small* 14, 1702926 (2018).
- 144. Park, M. et al. Skin-integrated systems for power efficient, programmable thermal sensations across large body areas. *Proc. Natl Acad. Sci.* **120**, e2217828120 (2023).
- 145. Grunwald, M. *Human Haptic Perception: Basics and Applications* (Birkhäuser Basel, 2008).
- Johansson, R. S. & Flanagan, J. R. Coding and use of tactile signals from the fingertips in object manipulation tasks. *Nat. Rev. Neurosci.* 10, 345–359 (2009).
- 147. Johansson, R. S. & Flanagan, J. R. in *Encyclopedia of Neuroscience* 583–594 (Elsevier, 2009).
- Bolanowski, S. J., Gescheider, G. A. & Verrillo, R. T. Hairy skin: psychophysical channels and their physiological substrates. *Somatosens. Mot. Res.* **11**, 279–290 (1994).
- Ackerley, R. et al. Touch perceptions across skin sites: differences between sensitivity, direction discrimination and pleasantness. *Front. Behav. Neurosci.* 8, 54 (2014).
- Johansson, R. S., Landström, U. & Lundström, R. Responses of mechanoreceptive afferent units in the glabrous skin of the human hand to sinusoidal skin displacements. *Brain Res.* 244, 17–25 (1982).
- 151. Löfvenberg, J. & Johansson, R. S. Regional differences and interindividual variability in sensitivity to vibration in the glabrous skin of the human hand. *Brain Res.* **301**, 65–72 (1984).
- Johansson, R. S. & Vallbo, Å. B. Tactile sensory coding in the glabrous skin of the human hand. *Trends Neurosci.* 6, 27–32 (1983).
- Brisben, A. J., Hsiao, S. S. & Johnson, K. O. Detection of vibration transmitted through an object grasped in the hand. *J. Neurophysiol.* 81, 1548–1558 (1999).
- Loewenstein, W. R. & Skalak, R. Mechanical transmission in a Pacinian corpuscle. An analysis and a theory. *J. Physiol.* 182, 346–378 (1966).
- Choi, S. & Kuchenbecker, K. J. Vibrotactile display: perception, technology, and applications. *Proc. IEEE* **101**, 2093–2104 (2013).
- 156. Gescheider, G. A. Psychophysics (Psychology Press, 2013).
- Gandhi, M. S., Sesek, R., Tuckett, R. & Bamberg, S. J. M. Progress in vibrotactile threshold evaluation techniques: a review. *J. Hand Ther.* 24, 240–256 (2011).
- Whitehouse, D. J. & Griffin, M. J. A comparison of vibrotactile thresholds obtained using different diagnostic equipment: the effect of contact conditions. *Int. Arch. Occup. Environ. Health* 75, 85–89 (2002).
- 159. Asano, S., Okamoto, S. & Yamada, Y. Vibrotactile stimulation to increase and decrease texture roughness. *IEEE Trans. Hum. -Mach. Syst.* **45**, 393–398 (2015).
- Konyo, M., Yamada, H., Okamoto, S. & Tadokoro, S. In *Haptics:* Perception, Devices and Scenarios (ed. Ferre, M.) 619–629 (Springer Berlin Heidelberg, 2008).
- Lindeman, R. W., Yanagida, Y., Noma, H. & Hosaka, K. Wearable vibrotactile systems for virtual contact and information display. *Virtual Real.* 9, 203–213 (2006).
- Ozioko, O., Karipoth, P., Hersh, M. & Dahiya, R. Wearable assistive tactile communication interface based on integrated touch sensors and actuators. *IEEE Trans. Neural Syst. Rehabil. Eng.* 28, 1344–1352 (2020).
- Ozioko, O., Navaraj, W., Hersh, M. & Dahiya, R. Tacsac: a wearable haptic device with capacitive touch-sensing capability for tactile display. *Sensors* 20, 4780 (2020).

- Altini, M., Farella E., Pirini, M. & Benini, L. A cost-effective indoor vibrotactile navigation system for the blind. in *Proc. International Conference on Health Informatics* 477–481 (SciTePress, 2011).
- Devigne, L. et al. Power wheelchair navigation assistance using wearable vibrotactile haptics. *IEEE Trans. Haptics* 13, 52–58 (2020).
- 166. Ju, Y. et al. Haptic empathy: conveying emotional meaning through vibrotactile feedback. in *Extended Abstracts of the 2021 CHI Conference on Human Factors in Computing Systems* 1–7 (ACM, 2021).
- 167. Ryu, J. et al. Vibrotactile feedback for information delivery in the vehicle. *IEEE Trans. Haptics* **3**, 138–149 (2010).
- Petermeijer, S. M., De Winter, J. C. F. & Bengler, K. J. Vibrotactile displays: a survey with a view on highly automated driving. *IEEE Trans. Intell. Transp. Syst.* **17**, 897–907 (2016).
- Guo, W., Hu, Y., Yin, Z. & Wu, H. On-skin stimulation devices for haptic feedback and human–machine interfaces. *Adv. Mater. Technol.* 7, 2100452 (2022).
- 170. Cha, J., Eid, M., Rahal, L. & El Saddik, A. Hugme: an interpersonal haptic communication system. In *2008 IEEE International Workshop on Haptic Audio visual Environments and Games* 99–102 (IEEE, 2008).
- 171. Lemmens, P. et al. A body-conforming tactile jacket to enrich movie viewing. in World Haptics 2009 – Third Joint EuroHaptics Conference and Symposium on Haptic Interfaces for Virtual Environment and Teleoperator Systems 7–12 (IEEE, 2009).
- 172. Bark, K. et al. Lessons in using vibrotactile feedback to guide fast arm motions. In *2011 IEEE World Haptics Conference* 355–360 (IEEE, 2011).
- 173. McDaniel, T. et al. Using a haptic belt to convey non-verbal communication cues during social interactions to individuals who are blind. In 2008 IEEE International Workshop on Haptic Audio visual Environments and Games 13–18 (IEEE, 2008).
- 174. Luo, H. et al. Hap-pulse: a wearable vibrotactile glove for medical pulse wave rendering. *IEEE Trans. Haptics* **15**, 280–291 (2022).
- 175. Rinderknecht, M. D. et al. Objective assessment of vibrotactile mislocalization using a Haptic Glove. In 2015 IEEE International Conference on Rehabilitation Robotics (ICORR) 145–150 (IEEE, 2015).
- 176. Yu, X. et al. Skin-integrated wireless haptic interfaces for virtual and augmented reality. *Nature* **575**, 473–479 (2019).
- 177. Liu, Y. et al. Electronic skin as wireless human-machine interfaces for robotic VR. *Sci. Adv.* **8**, eabl6700 (2022).
- 178. Li, D. et al. Touch IoT enabled by wireless self-sensing and hapticreproducing electronic skin. *Sci. Adv.* **8**, eade2450 (2022).
- Sonar, H. A., Huang, J.-L. & Paik, J. Soft touch using soft pneumatic actuator–skin as a wearable haptic feedback device. *Adv. Intell. Syst.* 3, 2000168 (2021).
- Kikkert, S. et al. Hand and face somatotopy shown using mri-safe vibrotactile stimulation with a novel soft pneumatic actuator (spa)skin interface. *NeuroImage* 269, 119932 (2023).
- Talhan, A., Kim, H. & Jeon, S. Wearable soft pneumatic ring with multi-mode controlling for rich haptic effects. in ACM SIGGRAPH 2019 Posters 1–2 (ACM, 2019).
- Sonar, H. A., Gerratt, A. P., Lacour, S. P. & Paik, J. Closed-loop haptic feedback control using a self-sensing soft pneumatic actuator skin. Soft Robot. 7, 22–29 (2020).
- Carpi, F., Bauer, S. & De Rossi, D. Stretching dielectric elastomer performance. Science 330, 1759–1761 (2010).
- Duduta, M., Wood, R. J. & Clarke, D. R. Multilayer dielectric elastomers for fast, programmable actuation without prestretch. *Adv. Mater.* 28, 8058–8063 (2016).
- Pei, Q. et al. Multiple-degrees-of-freedom electroelastomer roll actuators. Smart Mater. Struct. 13, N86–N92 (2004).

- Ji, X. et al. Untethered feel-through haptics using 18-μm thick dielectric elastomer actuators. *Adv. Funct. Mater.* 31, 2006639 (2021).
- Park, W.-H. et al. Soft haptic actuator based on knitted PVC gel fabric. *IEEE Trans. Ind. Electron.* 67, 677–685 (2020).
- Vedel, J. P. & Roll, J. P. Response to pressure and vibration of slowly adapting cutaneous mechanoreceptors in the human foot. *Neurosci. Lett.* 34, 289–294 (1982).
- HP Virtual Museum. Hewlett-Packard-150 Touchscreen Personal Computer with Hewlett-Packard 9121 Dual Drives. https://www.hp. com/hpinfo/abouthp/histnfacts/museum/personalsystems/ 0031/ (1983).
- Charalambides, A. & Bergbreiter, S. Rapid manufacturing of mechanoreceptive skins for slip detection in robotic grasping. *Adv. Mater. Technol.* 2, 1600188 (2017).
- Koivikko, A. et al. Screen-printed curvature sensors for soft robots. IEEE Sens. J. 18, 223–230 (2018).
- 192. Yang, Y. & Gao, W. Wearable and flexible electronics for continuous molecular monitoring. *Chem. Soc. Rev.* **48**, 1465–1491 (2019).
- Viventi, J. et al. A conformal, bio-interfaced class of silicon electronics for mapping cardiac electrophysiology. *Sci. Transl. Med.* 2, 24ra22 (2010).
- 194. Gao, W. et al. Fully integrated wearable sensor arrays for multiplexed in situ perspiration analysis. *Nature* **529**, 509–514 (2016).
- 195. Sekitani, T. et al. A rubberlike stretchable active matrix using elastic conductors. *Science* **321**, 1468–1472 (2008).
- Pan, L. et al. An ultra-sensitive resistive pressure sensor based on hollow-sphere microstructure induced elasticity in conducting polymer film. *Nat. Commun.* 5, 3002 (2014).
- 197. Li, Y. et al. Smart glove integrated with tunable MWNTS/pDMS fibers made of a one-step extrusion method for finger dexterity, gesture, and temperature recognition. ACS Appl. Mater. Interfaces **12**, 23764–23773 (2020).
- Harada, S. et al. Fully printed flexible fingerprint-like three-axis tactile and slip force and temperature sensors for artificial skin. ACS Nano 8, 12851–12857 (2014).
- Toriyama, T. & Sugiyama, S. Analysis of piezoresistance in p-type silicon for mechanical sensors. *J. Microelectromechanical Syst.* **11**, 598–604 (2002).
- Tombler, T. W. et al. Reversible electromechanical characteristics of carbon nanotubes underlocal-probe manipulation. *Nature* 405, 769–772 (2000).
- Bae, S.-H. et al. Graphene-based transparent strain sensor. *Carbon* 51, 236–242 (2013).
- Yang, T. et al. Tactile sensing system based on arrays of graphene woven microfabrics: electromechanical behavior and electronic skin application. ACS Nano 9, 10867–10875 (2015).
- Yi, C. et al. Highly sensitive and wide linear-response pressure sensors featuring zero standby power consumption under bending conditions. ACS Appl. Mater. Interfaces 12, 19563–19571 (2020).
- Park, J. et al. Tactile-direction-sensitive and stretchable electronic skins based on human-skin-inspired interlocked microstructures. ACS Nano 8, 12020–12029 (2014).
- 205. Gao, Y. et al. Wearable microfluidic diaphragm pressure sensor for health and tactile touch monitoring. *Adv. Mater.* **29**, 1701985 (2017).
- Xi, W. et al. Ultrathin and wearable microtubular epidermal sensor for real-time physiological pulse monitoring. *Adv. Mater. Technol.* 2, 1700016 (2017).
- Kang, D. et al. Ultrasensitive mechanical crack-based sensor inspired by the spider sensory system. *Nature* 516, 222–226 (2014).
- Timsit, S. Electrical contact resistance: properties of stationary interfaces. In *Electrical Contacts* – 1998. Proceedings of the Forty-Fourth IEEE Holm Conference on Electrical Contacts (Cat. No.98CB36238) 1–19 (IEEE, 1998).

- Yamada, T. et al. A stretchable carbon nanotube strain sensor for human-motion detection. *Nat. Nanotechnol.* 6, 296–301 (2011).
- Mannsfeld, S. C. B. et al. Highly sensitive flexible pressure sensors with microstructured rubber dielectric layers. *Nat. Mater.* 9, 859–864 (2010).
- Lee, H.-K., Chung, J., Chang, S.-I. & Yoon, E. Real-time measurement of the three-axis contact force distribution using a flexible capacitive polymer tactile sensor. *J. Micromech. Microeng.* 21, 035010 (2011).
- Lipomi, D. J. et al. Skin-like pressure and strain sensors based on transparent elastic films of carbon nanotubes. *Nat. Nanotechnol.* 6, 788–792 (2011).
- 213. Puers, R. Capacitive sensors: when and how to use them. Sens. Actuators Phys. **37–38**, 93–105 (1993).
- Muhammad, H. B. et al. A capacitive tactile sensor array for surface texture discrimination. *Microelectron. Eng.* 88, 1811–1813 (2011).
- 215. Cheng, M.-Y., Lin, C.-L., Lai, Y.-T. & Yang, Y.-J. A polymer-based capacitive sensing array for normal and shear force measurement. *Sensors* **10**, 10211–10225 (2010).
- Ponce Wong, R. D., Posner, J. D. & Santos, V. J. Flexible microfluidic normal force sensor skin for tactile feedback. *Sens. Actuators Phys.* 179, 62–69 (2012).
- 217. Zang, Y. et al. Flexible suspended gate organic thin-film transistors for ultra-sensitive pressure detection. *Nat. Commun.* **6**, 6269 (2015).
- Sharma, S. et al. Wearable capacitive pressure sensor based on mxene composite nanofibrous scaffolds for reliable human physiological signal acquisition. ACS Appl. Mater. Interfaces 12, 22212–22224 (2020).
- Persano, L. et al. High performance piezoelectric devices based on aligned arrays of nanofibers of poly(vinylidenefluoride-cotrifluoroethylene). *Nat. Commun.* 4, 1633 (2013).
- 220. Wu, W., Wen, X. & Wang, Z. L. Taxel-addressable matrix of verticalnanowire piezotronic transistors for active and adaptive tactile imaging. *Science* **340**, 952–957 (2013).
- Sun, Q. et al. Active matrix electronic skin strain sensor based on piezopotential-powered graphene transistors. *Adv. Mater.* 27, 3411–3417 (2015).
- 222. Graz, I. et al. Flexible active-matrix cells with selectively poled bifunctional polymer-ceramic nanocomposite for pressure and temperature sensing skin. *J. Appl. Phys.* **106**, 034503 (2009).
- Pi, Z. et al. Flexible piezoelectric nanogenerator made of poly(vinylidenefluoride-co-trifluoroethylene) (PVDF-TrFE) thin film. *Nano Energy* 7, 33–41 (2014).
- 224. Bhavanasi, V. et al. Enhanced piezoelectric energy harvesting performance of flexible pvdf-trfe bilayer films with graphene oxide. *ACS Appl. Mater. Interfaces* **8**, 521–529 (2016).
- 225. Chen, X. et al. Flexible three-axial tactile sensors with microstructure-enhanced piezoelectric effect and speciallyarranged piezoelectric arrays. *Smart Mater. Struct.* **27**, 025018 (2018).
- 226. Hirohata, A. et al. Review on spintronics: Principles and device applications. *J. Magn. Magn. Mater.* **509**, 166711 (2020).
- 227. Khan, M. A. et al. Magnetic sensors-a review and recent technologies. *Eng. Res. Express* **3**, 022005 (2021).
- 228. George, B., Tan, Z. & Nihtianov, S. Advances in capacitive, eddy current, and magnetic displacement sensors and corresponding interfaces. *IEEE Trans. Ind. Electron.* **64**, 9595–9607 (2017).
- 229. Tomo, T. P. et al. Covering a robot fingertip with uSkin: a soft electronic skin with distributed 3-axis force sensitive elements for robot hands. *IEEE Robot. Autom. Lett.* **3**, 124–131 (2018).
- 230. Ribeiro, P. et al. Bioinspired ciliary force sensor for robotic platforms. *IEEE Robot. Autom. Lett.* **2**, 971–976 (2017).
- 231. Alfadhel, A., Khan, M. A., Cardoso De Freitas, S. & Kosel, J. Magnetic tactile sensor for braille reading. *IEEE Sens. J.* **16**, 8700–8705 (2016).

- Ribeiro, P., Cardoso, S., Bernardino, A. & Jamone, L. Highly sensitive bio-inspired sensor for fine surface exploration and characterization. in 2020 IEEE International Conference on Robotics and Automation (ICRA) 625–631 (IEEE, 2020).
- Yi, Z., Zhang, Y. & Peters, J. Bioinspired tactile sensor for surface roughness discrimination. *Sens. Actuators Phys.* 255, 46–53 (2017).
- 234. Oh, S. et al. Remote tactile sensing system integrated with magnetic synapse. *Sci. Rep.* **7**, 16963 (2017).
- Chathuranga, D. S. et al. Disposable soft 3 axis force sensor for biomedical applications. In 2015 37th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC) 5521–5524 (IEEE, 2015).
- Li, Y. et al. The progress of magnetic sensor applied in biomedicine: a review of non-invasive techniques and sensors. *J. Chin. Chem. Soc.* 68, 216–227 (2021).
- 237. Yan, Y. et al. Soft magnetic skin for super-resolution tactile sensing with force self-decoupling. *Sci. Robot.* **6**, eabc8801 (2021).
- Youssefian, S., Rahbar, N. & Torres-Jara, E. Contact behavior of soft spherical tactile sensors. *IEEE Sens. J.* 14, 1435–1442 (2014).
- Jamone, L., Natale, L., Metta, G. & Sandini, G. Highly sensitive soft tactile sensors for an anthropomorphic robotic hand. *IEEE Sens. J.* 15, 4226–4233 (2015).
- Yu, P., Qi, X., Liu, W. & Fu, X. Development of a compliant magnetic 3-d tactile sensor with amr elements. In *Intelligent Robotics and Applications* (eds. Zhang, X., Liu, H., Chen, Z. & Wang, N.)484–491 (Springer International Publishing, 2014).
- 241. Kim, S.-H. et al. Design of a bioinspired robotic hand: magnetic synapse sensor integration for a robust remote tactile sensing. *IEEE Robot. Autom. Lett.* **3**, 3545–3552 (2018).
- Goka, M., Nakamoto, H. & Takenawa, S. A magnetic type tactile sensor by GMR elements and inductors. In 2010 IEEE/RSJ International Conference on Intelligent Robots and Systems 885–890 (IEEE, 2010).
- Hale, K. & Flatau, A. Galfenol tactile sensor array and visual mapping system. in (ed. Matsuzaki, Y.) 61730Y (Astrophysics Data System, 2006).
- 244. Nakamoto, H., Takenawa, S. & Kida, Y. Structure and fundamental evaluation of magnetic type tactile sensor. *Int. J. Appl. Electromagn. Mech.* **39**, 1021–1026 (2012).
- Nakamoto, H. & Matsumoto, T. Tactile texture classification using magnetic tactile sensor. *Int. J. Appl. Electromagn. Mech.* 52, 1673–1679 (2016).
- Rosle, Wang & Hirai Geometry optimisation of a hall-effect-based soft fingertip for estimating orientation of thin rectangular objects. *Sensors* 19, 4056 (2019).
- Alfadhel, A., Khan, M. A., Cardoso, S. & Kosel, J. A single magnetic nanocomposite cilia force sensor. In 2016 IEEE Sensors Applications Symposium (SAS) 1–4 (IEEE, 2016).
- Park, J. J., Reddy, K. S. M., Stadler, B. & Flatau, A. Magnetostrictive fe–ga/cu nanowires array with GMR sensor for sensing applied pressure. *IEEE Sens. J.* 17, 2015–2020 (2017).
- 249. Holgado, A. C. et al. Improvements on a sensitivity adjustable 3-axis soft skin sensor with an electromagnet. In *2020 IEEE/SICE International Symposium on System Integration (SII)* 68–73 (IEEE, 2020).
- Wattanasarn, S., Noda, K., Matsumoto, K. & Shimoyama, I. 3D flexible tactile sensor using electromagnetic induction coils. In 2012 IEEE 25th International Conference on Micro Electro Mechanical Systems (MEMS) 488–491 (IEEE, 2012).
- Zhang, F. et al. Flexible and self-powered temperature-pressure dual-parameter sensors using microstructure-frame-supported organic thermoelectric materials. *Nat. Commun.* 6, 8356 (2015).
- 252. Wang, Y., Zhang, S. M. & Deng, Y. Flexible low-grade energy utilization devices based on high-performance thermoelectric

polyaniline/tellurium nanorod hybrid films. *J. Mater. Chem. A* **4**, 3554–3559 (2016).

- 253. Xu, P. A. et al. Optical lace for synthetic afferent neural networks. *Sci. Robot.* **4**, eaaw6304 (2019).
- 254. Heo, J.-S., Kim, K.-Y. & Lee, J.-J. Development of a distributed force detectable artificial skin using microbending optical fiber sensors. *J. Intell. Mater. Syst. Struct.* **20**, 2029–2036 (2009).
- 255. Rothmaier, M., Luong, M. & Clemens, F. Textile pressure sensor made of flexible plastic optical fibers. *Sensors* **8**, 4318–4329 (2008).
- Van Meerbeek, I. M., De Sa, C. M. & Shepherd, R. F. Soft optoelectronic sensory foams with proprioception. *Sci. Robot.* 3, eaau2489 (2018).
- 257. Fan, F.-R. et al. Transparent triboelectric nanogenerators and selfpowered pressure sensors based on micropatterned plastic films. *Nano Lett.* **12**, 3109–3114 (2012).
- 258. Zhao, X. et al. Polyimide/graphene nanocomposite foam-based wind-driven triboelectric nanogenerator for self-powered pressure sensor. *Adv. Mater. Technol.* **4**, 1800723 (2019).
- 259. Zhu, G. et al. Self-powered, ultrasensitive, flexible tactile sensors based on contact electrification. *Nano Lett.* **14**, 3208–3213 (2014).
- 260. Yang, J. C. et al. Electronic skin: recent progress and future prospects for skin-attachable devices for health monitoring, robotics, and prosthetics. *Adv. Mater.* **31**, 1904765 (2019).
- Kim, J.-O. et al. Highly ordered 3d microstructure-based electronic skin capable of differentiating pressure, temperature, and proximity. ACS Appl. Mater. Interfaces 11, 1503–1511 (2019).
- Kaboli, M., Long, A. & Cheng, G. Humanoids learn touch modalities identification via multi-modal robotic skin and robust tactile descriptors. *Adv. Robot.* 29, 1411–1425 (2015).
- Wang, Z. et al. Flexible hemispheric microarrays of highly pressuresensitive sensors based on breath figure method. *Nanoscale* 10, 10691–10698 (2018).
- Bae, G. Y. et al. Linearly and highly pressure-sensitive electronic skin based on a bioinspired hierarchical structural array. *Adv. Mater.* 28, 5300–5306 (2016).
- 265. Lee, Y. et al. Flexible ferroelectric sensors with ultrahigh pressure sensitivity and linear response over exceptionally broad pressure range. *ACS Nano* **12**, 4045–4054 (2018).
- Oh, J. et al. Highly uniform and low hysteresis piezoresistive pressure sensors based on chemical grafting of polypyrrole on elastomer template with uniform pore size. *Small* 15, 1901744 (2019).
- 267. Chortos, A., Liu, J. & Bao, Z. Pursuing prosthetic electronic skin. *Nat. Mater.* **15**, 937–950 (2016).
- 268. Li, X. et al. Stretchable and highly sensitive graphene-on-polymer strain sensors. *Sci. Rep.* **2**, 870 (2012).
- 269. Sui, C. et al. Directional sensing based on flexible aligned carbon nanotube film nanocomposites. *Nanoscale* **10**, 14938–14946 (2018).
- Amjadi, M. et al. Highly stretchable and sensitive strain sensor based on silver nanowire–elastomer nanocomposite. ACS Nano 8, 5154–5163 (2014).
- Yoon, S. G., Park, B. J. & Chang, S. T. Highly sensitive microfluidic strain sensors with low hysteresis using a binary mixture of ionic liquid and ethylene glycol. *Sens. Actuators Phys.* 254, 1–8 (2017).
- 272. Chen, J. et al. A liquid metal based super-stretchable strain sensor. In 2018 IEEE 13th Annual International Conference on Nano/Micro Engineered and Molecular Systems (NEMS) 377–380 (IEEE, 2018).
- Jeon, S. et al. Flexible multimodal sensors for electronic skin: principle, materials, device, array architecture, and data acquisition method. *Proc. IEEE* **107**, 2065–2083 (2019).
- 274. Kaltenbrunner, M. et al. An ultra-lightweight design for imperceptible plastic electronics. *Nature* **499**, 458–463 (2013).
- Webb, R. C. et al. Ultrathin conformal devices for precise and continuous thermal characterization of human skin. *Nat. Mater.* 12, 938–944 (2013).

- 276. Chen, Y., Lu, B., Chen, Y. & Feng, X. Breathable and stretchable temperature sensors inspired by skin. *Sci. Rep.* **5**, 11505 (2015).
- Yokota, T. et al. Ultraflexible, large-area, physiological temperature sensors for multipoint measurements. *Proc. Natl Acad. Sci.* **112**, 14533–14538 (2015).
- 278. Someya, T. et al. Conformable, flexible, large-area networks of pressure and thermal sensors with organic transistor active matrixes. *Proc. Natl Acad. Sci.* **102**, 12321–12325 (2005).
- Johansson, R. S. & Westling, G. Roles of glabrous skin receptors and sensorimotor memory in automatic control of precision grip when lifting rougher or more slippery objects. *Exp. Brain Res.* 56, 550–564 (1984).
- Cadoret, G. & Smith, A. M. Friction, not texture, dictates grip forces used during object manipulation. *J. Neurophysiol.* 75, 1963–1969 (1996).
- 281. Viry, L. et al. Flexible three-axial force sensor for soft and highly sensitive artificial touch. *Adv. Mater.* **26**, 2659–2664 (2014).
- Shang, C. et al. Multi-parameter e-skin based on biomimetic mechanoreceptors and stress field sensing. *Npj Flex. Electron.* 7, 19 (2023).
- Lee, J.-I., Pyo, S., Kim, M.-O. & Kim, J. Multidirectional flexible force sensors based on confined, self-adjusting carbon nanotube arrays. *Nanotechnology* 29, 055501 (2018).
- Ribeiro, P., Cardoso, S., Bernardino, A. & Jamone, L. Fruit quality control by surface analysis using a bio-inspired soft tactile sensor. In 2020 IEEE/RSJ International Conference on Intelligent Robots and Systems (IROS) 8875–8881 (IEEE, 2020).
- Carvalho, M., Ribeiro, P., Romão, V. & Cardoso, S. Smart fingertip sensor for food quality control: Fruit maturity assessment with a magnetic device. *J. Magn. Magn. Mater.* **536**, 168116 (2021).
- Zhu, M. et al. Soft, wearable robotics and haptics: technologies, trends, and emerging applications. *Proc. IEEE* 110, 246–272 (2022).
- Marechal, L. et al. Toward a common framework and database of materials for soft robotics. Soft Robot. 8, 284–297 (2021).
- Biswas, S. & Visell, Y. Emerging material technologies for haptics. Adv. Mater. Technol. 4, 1900042 (2019).
- 289. Green, B. G. The effect of skin temperature on vibrotactile sensitivity. *Percept. Psychophys.* **21**, 243–248 (1977).
- Harazin, B. & Harazin-Lechowska, A. Effect of changes in finger skin temperature on vibrotactile perception threshold. *Int. J. Occup. Med. Environ. Health* **20**, 223–227 (2007).
- Green, B., Lederman, S. & Stevens, J. The effect of skin temperature on the perception of roughness. *Sens. Process.* 3, 327–333 (1980).
- Craig, A. D. & Bushnell, M. C. The thermal grill illusion: unmasking the burn of cold pain. *Science* 265, 252–255 (1994).
- Leung, A. Y., Wallace, M. S., Schulteis, G. & Yaksh, T. L. Qualitative and quantitative characterization of the thermal grill. *Pain* **116**, 26–32 (2005).
- 294. Lederman, S. J. Improving one's touch. *Percept. Psychophys.* 24, 154–160 (1978).
- Kikuuwe, R. et al. Enhancing haptic detection of surface undulation. ACM Trans. Appl. Percept. 2, 46–67 (2005).
- 296. G. H. Yang, K. U. Kyung, Srinivasan, M. A., & D. S. Kwon Quantitative tactile display device with pin-array type tactile feedback and thermal feedback. in *Proc. 2006 IEEE International Conference on Robotics and Automation, 2006.* 3917–3922 (IEEE, 2006).
- 297. Kurogi, T. et al. Small, soft, thin, lightweight and flexible tactile display enabling to provide multiple mechanical stimuli. in *Extended Abstracts of the 2020 CHI Conference on Human Factors in Computing Systems* 1–8 (ACM, 2020).
- Hosoi, J., Ban, Y., Ito, K. & Warisawa, S. Pseudo-wind perception induced by cross-modal reproduction of thermal, vibrotactile, visual, and auditory stimuli. *IEEE Access* **11**, 4781–4793 (2023).
- 299. Yang, T.-H. et al. Design of flexible hybrid tactile display using electro-vibration and electroactive polymer modules. in *Volume 1:*

Development and Characterization of Multifunctional Materials; Modeling, Simulation and Control of Adaptive Systems; Integrated System Design and Implementation V001T03A034 (American Society of Mechanical Engineers, 2013).

- Kyung, K.-U., Ahn, M., Kwon, D.-S. & Srinivasan, M. A. A compact planar distributed tactile display and effects of frequency on texture judgment. *Adv. Robot.* **20**, 563–580 (2006).
- Huang, Y. et al. A skin-integrated multimodal haptic interface for immersive tactile feedback. *Nat. Electron.* 6, 1041 (2023).
- Sun, Z., Zhu, M., Shan, X. & Lee, C. Augmented tactile-perception and haptic-feedback rings as human-machine interfaces aiming for immersive interactions. *Nat. Commun.* 13, 5224 (2022).
- Yao, K. et al. Encoding of tactile information in hand via skin-integrated wireless haptic interface. *Nat. Mach. Intell.* 4, 893–903 (2022).
- Jung, Y. H. et al. A wireless haptic interface for programmable patterns of touch across large areas of the skin. *Nat. Electron.* 5, 374–385 (2022).
- Chen, D., Lou, Z., Jiang, K. & Shen, G. Device configurations and future prospects of flexible/stretchable lithium-ion batteries. *Adv. Funct. Mater.* 28, 1805596 (2018).
- Kaltenbrunner, M. et al. Arrays of ultracompliant electrochemical dry gel cells for stretchable electronics. *Adv. Mater.* 22, 2065–2067 (2010).
- Li, Y. et al. Atomically thin mesoporous Co₃ O₄ layers strongly coupled with N-rGO nanosheets as high-performance bifunctional catalysts for 1D knittable zinc–air batteries. *Adv. Mater.* **30**, 1703657 (2018).
- Zhou, K. et al. Ultra-stretchable triboelectric nanogenerator as highsensitive and self-powered electronic skins for energy harvesting and tactile sensing. *Nano Energy* **70**, 104546 (2020).
- Wang, J. et al. A stretchable self-powered triboelectric tactile sensor with EGaln alloy electrode for ultra-low-pressure detection. *Nano Energy* 89, 106320 (2021).
- Vuong, N. H. L. et al. Active skin as a new haptic interface. in *Proc. of the SPIE* Vol. 7642 (ed. Bar-Cohen, Y.) 76422M (Astrophysics Data System, 2010).
- Robinson, S. S. et al. Integrated soft sensors and elastomeric actuators for tactile machines with kinesthetic sense. *Extrem. Mech. Lett.* 5, 47–53 (2015).
- Khin, P. M. et al. Soft haptics using soft actuator and soft sensor. In 2016 6th IEEE International Conference on Biomedical Robotics and Biomechatronics (BioRob) 1272–1276 (IEEE, 2016).
- Kadooka, K., Imamura, H. & Taya, M. Tactile sensor integrated dielectric elastomer actuator for simultaneous actuation and sensing. In *Proc. Volume 9798, Electroactive Polymer Actuators and Devices (EAPAD)* (eds. Bar-Cohen, Y. & Vidal, F.) 97982H (SPIE, 2016).
- Yun, S. et al. Polymer-based flexible visuo-haptic display. *IEEE* ASME Trans. Mechatron. 19, 1463–1469 (2014).
- 315. Phung, H. et al. Interactive haptic display based on soft actuator and soft sensor. in 2017 IEEE/RSJ International Conference on Intelligent Robots and Systems (IROS) 886–891 (IEEE, 2017).
- Phung, H. et al. Haptic display responsive to touch driven by soft actuator and soft sensor. *IEEE ASME Trans. Mechatron.* 26, 2495–2505 (2021).
- 317. Liu, N. et al. Ultratransparent and stretchable graphene electrodes. *Sci. Adv.* **3**, e1700159 (2017).
- Lee, P. et al. Highly stretchable or transparent conductor fabrication by a hierarchical multiscale hybrid nanocomposite. *Adv. Funct. Mater.* 24, 5671–5678 (2014).
- Jang, J. et al. Rapid production of large-area, transparent and stretchable electrodes using metal nanofibers as wirelessly operated wearable heaters. NPG Asia Mater. 9, e432–e432 (2017).
- 320. Oh, J. et al. A liquid metal based multimodal sensor and haptic feedback device for thermal and tactile sensation generation in virtual reality. *Adv. Funct. Mater.* **31**, 2007772 (2021).

This work is supported by the National Natural Science Foundation of China under Grant 62373021 and 62002185.

Author contributions

The authors' contributions to this review are as follows: Initial conception: D.W. and Y.G. Guidance: D.W. and Y.Z. Literature search and assembly: B.S. Writing: Y.G., Y.W., Q.T., D.W. Figures and table: B.S. and L.H. Editing: Y.G., Y.W., Q.T., D.W. These authors contributed equally: Y.G., Y.W., Q.T.

Competing interests

The authors declare no competing interests.

Additional information

Correspondence and requests for materials should be addressed to Dangxiao Wang.

Reprints and permissions information is available at

http://www.nature.com/reprints

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/.

© The Author(s) 2024